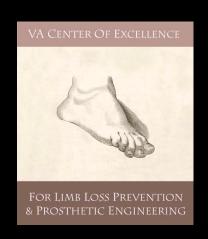




## Development of a biplane fluoroscope at the VA Puget Sound

William R. Ledoux, Joseph M. Iaquinto, Richard Tsai, Bruce Sangeorzan, Grant Marchelli, Matthew Kindig, Eric Thorhauer, Duane Storti, and David Haynor



RR&D Center of Excellence for Limb Loss Prevention and Prosthetic Engineering, VA Puget Sound



Departments of Mechanical Engineering, Radiology, Orthopaedics & Sports Medicine, University of Washington

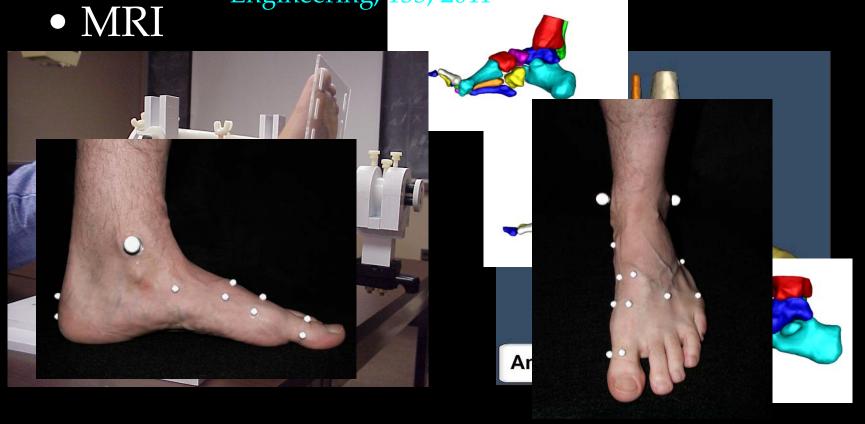






# Motivation for biplane fluoroscope development

• CT Weblittink of WRIC cetterly, I Warth of the Resistanche, 124, 126016w 2011 Engineering, 133, 2011









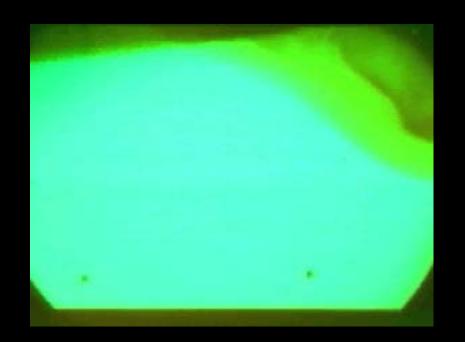
Arndt et al., 2007

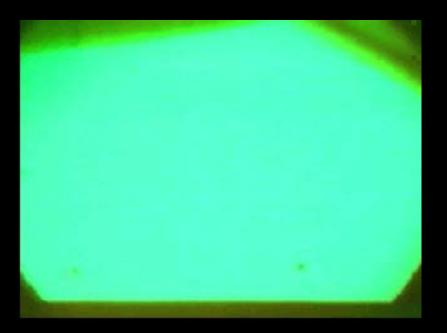
Invasive; not used for routine clinical care



## Fluoroscopy systems







De Clercq et al., 1994

Single plane; exposure to radiation



## Fluoroscopy systems





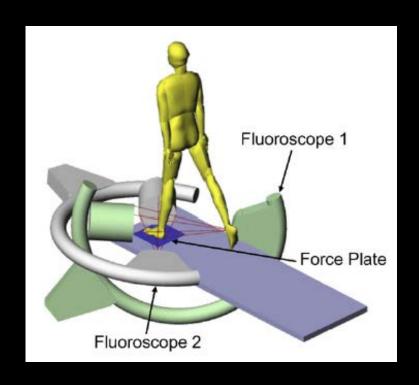
Yamaguchi et al., 2009

hindfoot only; exposure to radiation; 3D-2D



## Fluoroscopy systems







Li et al., 2008

Caputo et al., 2009

Portion of stance; exposure to radiation







- Custom biplane room too expensive
  - Henry Ford Hospital, U Pittsburgh, Brown
- C-arms
  - Mass General Hospital, Duke
- Modify existing C-arms
  - Steadman-Philippon Research Institute
- Hardware:
  - Two Philips BV-Pulsera C-arms
- Software:
  - Customized













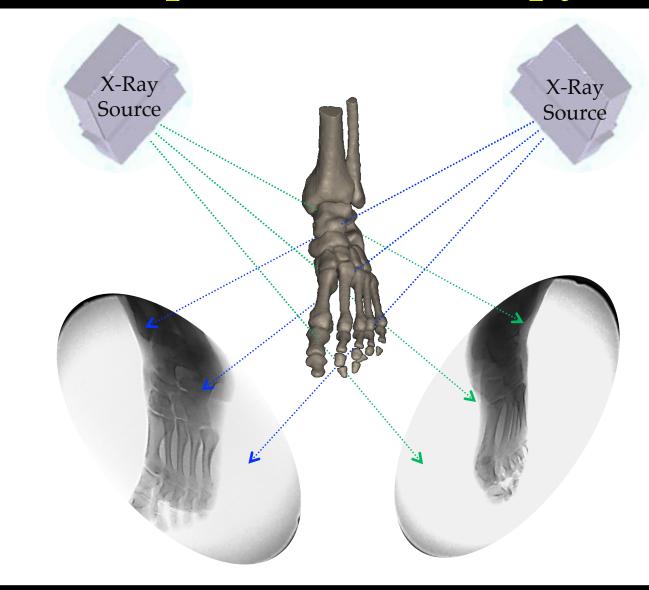














## Foot phantom







www.phantomlab.com



## Dynamic data collection

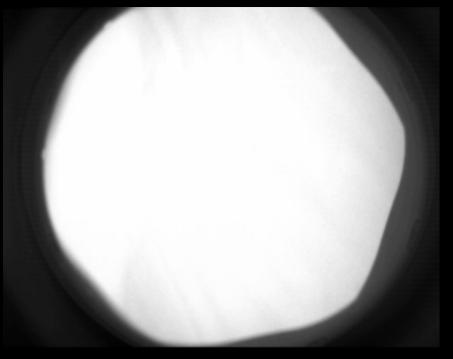














### Philips BV Pulsera C-Arms



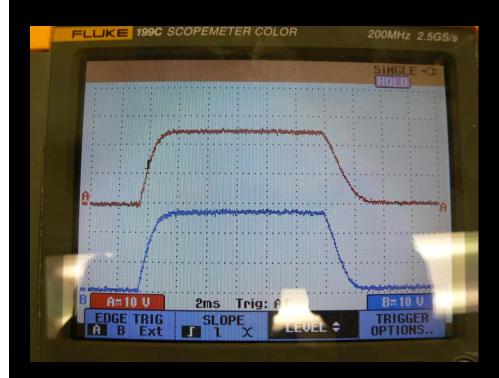
- Typical hospital C-arm
- 30 pulses/s or continuous

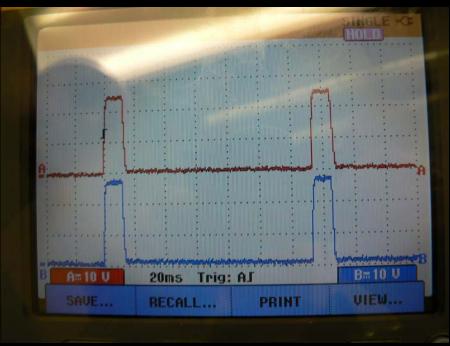




### Synchronizing systems



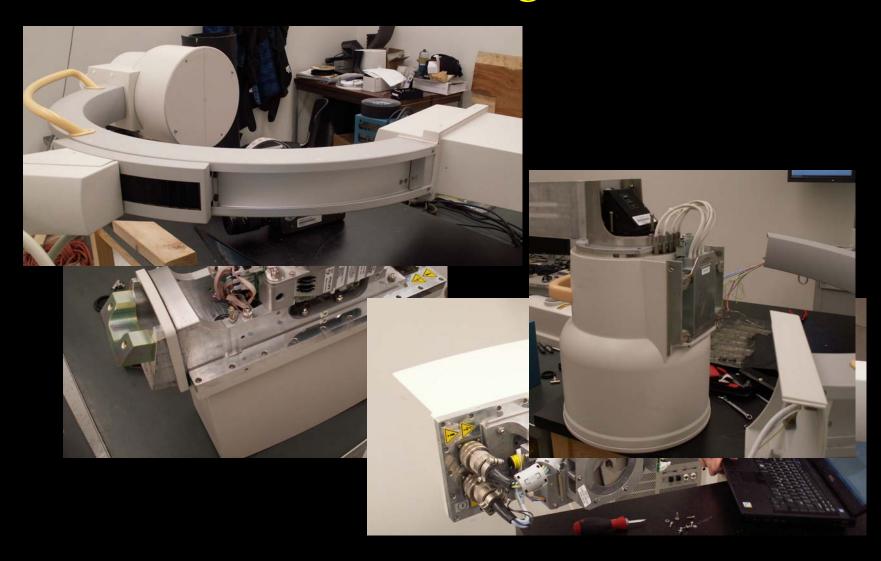






## Disassembling C-arms

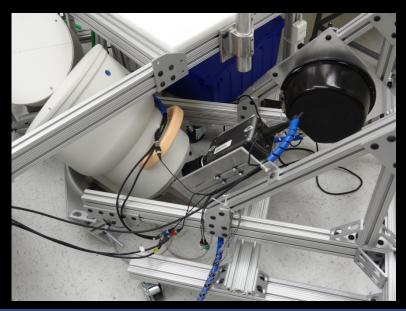


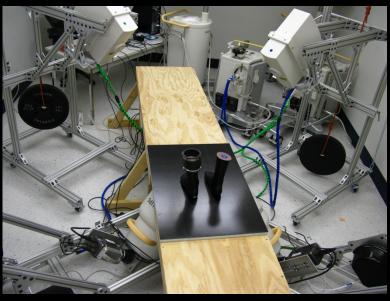


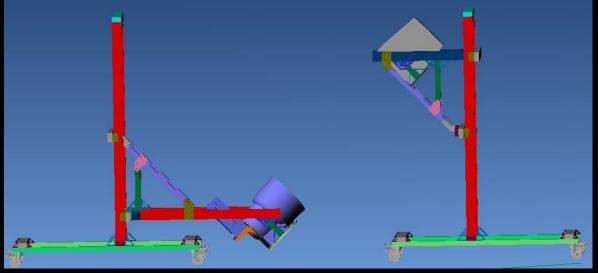


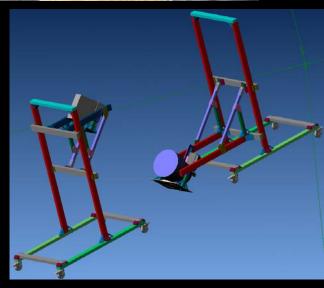
## Custom mounting devices













## Replacing cameras













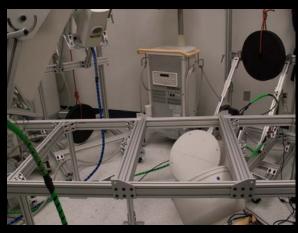


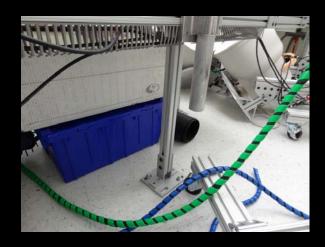


#### Final floor



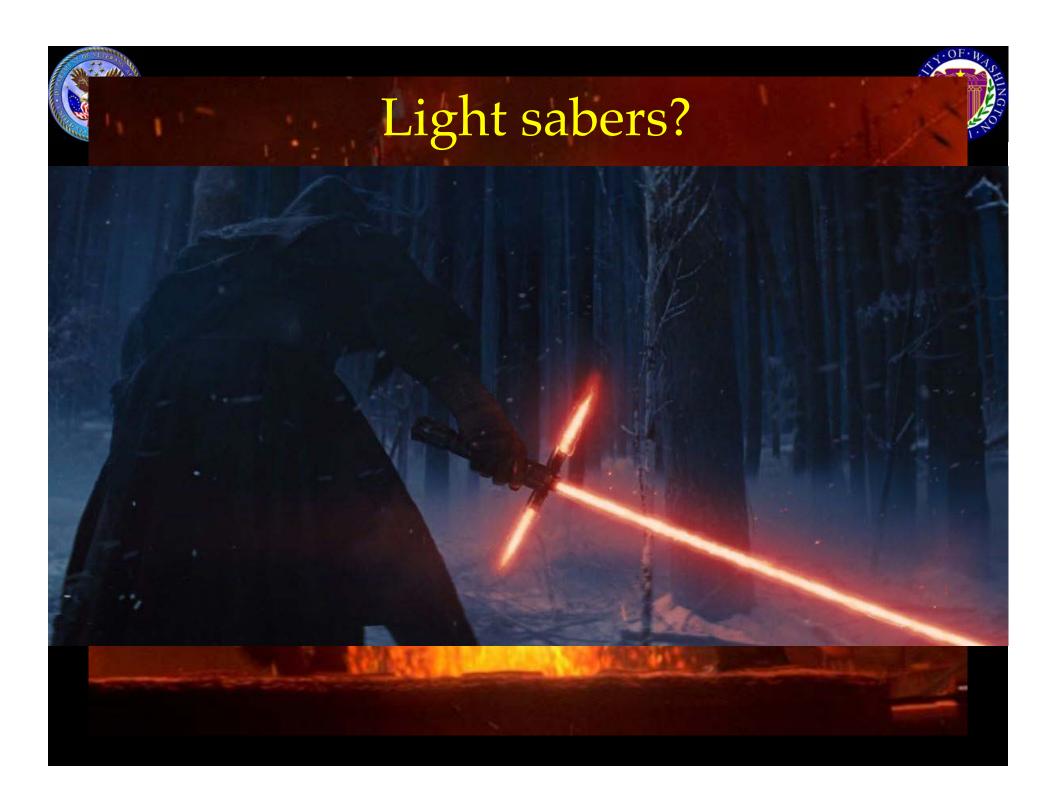














## Laser alignment











#### Customized software

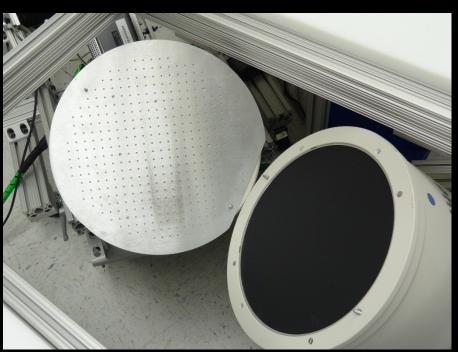


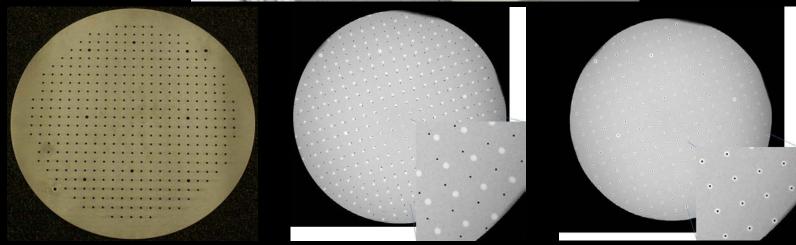
- Matlab, C/C++, CUDA
- Phase I: distortion and bias correction,
  3D calibration
- Phase II: generation of digital reconstructed radiographs (DRRs)
- Phase III: implementation of similarity measures and comparison methods
- Phase IV: speed and memory optimization



#### Distortion correction



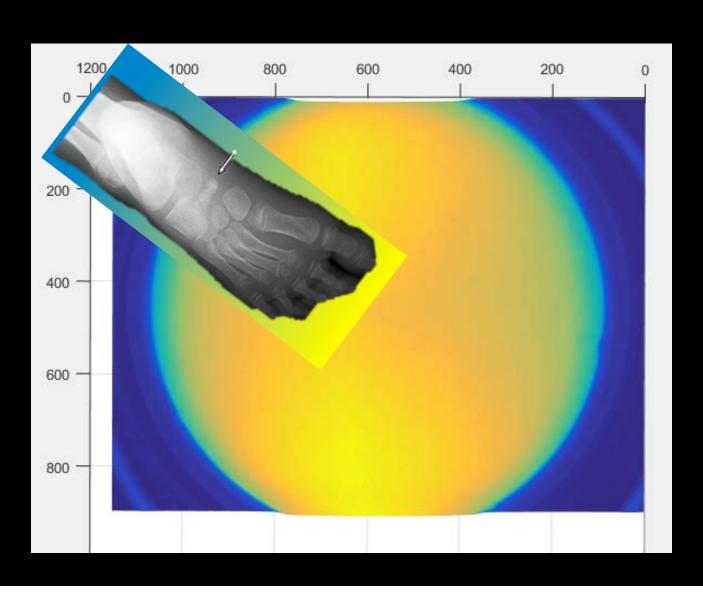






#### Flat-field correction

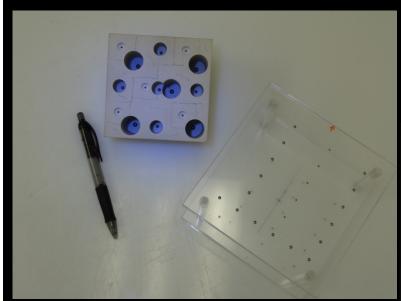


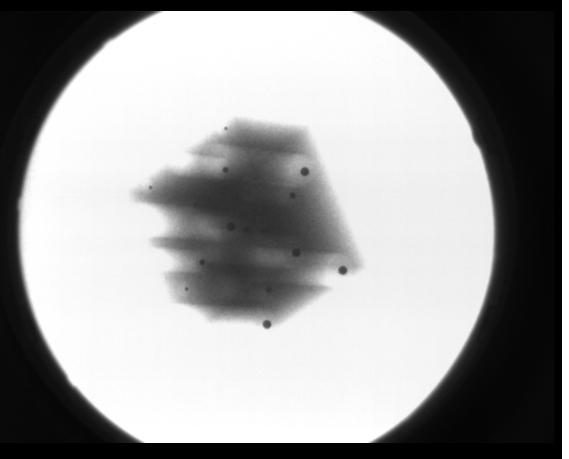




#### 3D Calibration



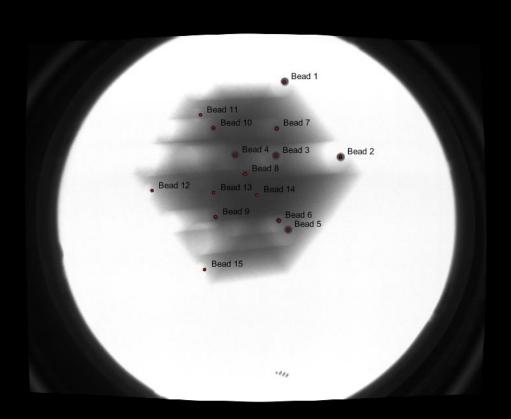


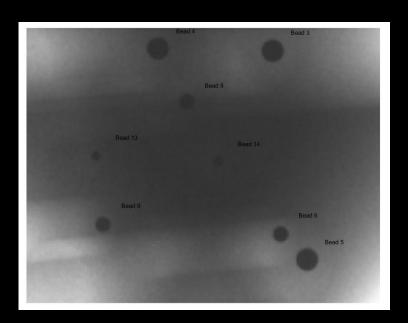


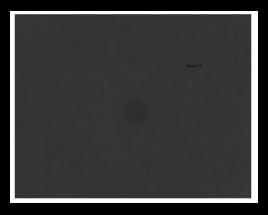


#### 3D calibration revised









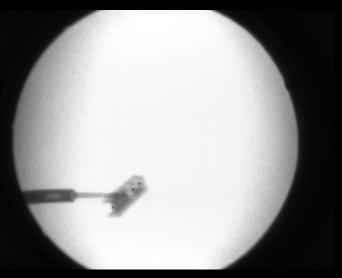


#### Validation: Bead-based



- Machined block or "wand"
  - 1.6mm tantalum beads
  - measured within 7 microns
- Wand translated and rotated via a 1 micron precision stepper-motor (static testing)
- Wand manually waved though FOV at ~0.5m/s (dynamic testing)

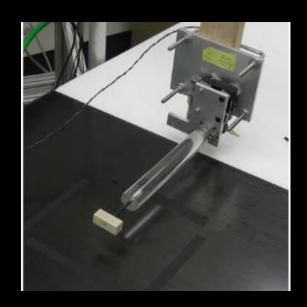






#### Validation: Bead-based, Static



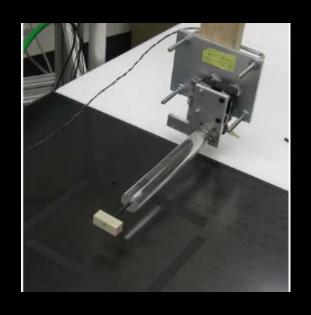






- Average translational accuracy = 0.0811 mm
- Average translational precision =  $\pm 0.0103$  mm
- Average rotational accuracy = 0.1541°
- Average rotation precision =  $\pm$  0.1382 °

## Validation: Bead-based, Dynamic







- Average accuracy = 0.1260 mm
- Average precision =  $\pm$  0.1218 mm



#### Validation: Bone-based



- Bones in foam block
  - 1.6mm tantalum beads

• Block translated and rotated via a 1 micron

precision

 Block ma (dynamic at  $\sim 1 \text{ m/s}$ 

Α

В



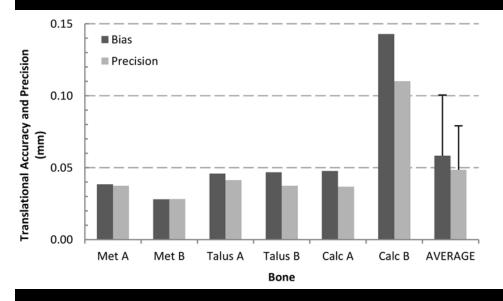
#### Validation: Bone-based, Static

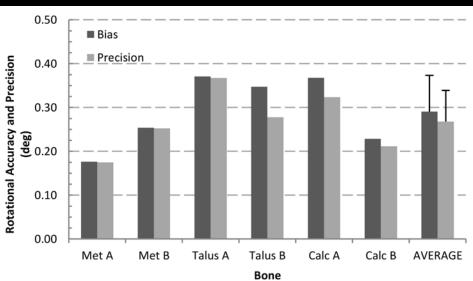








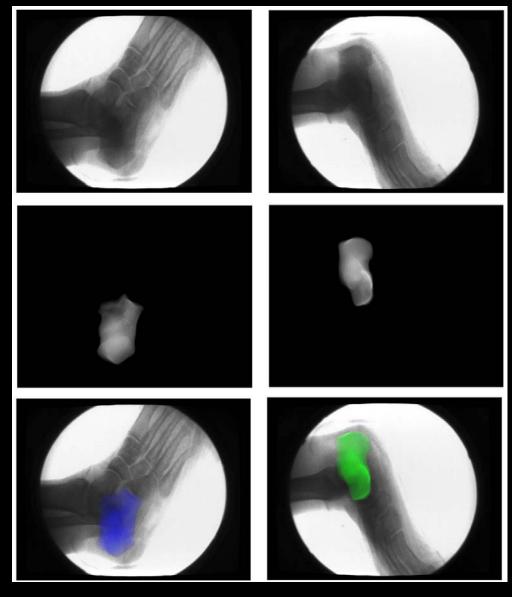








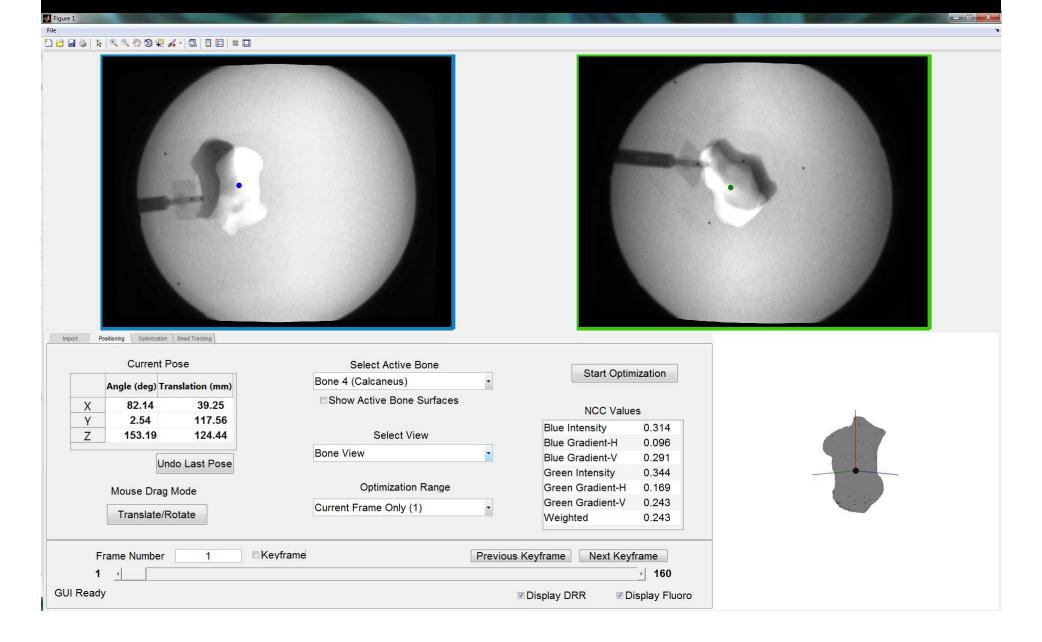






## GUI: unoptimized







#### GUI: optimized



