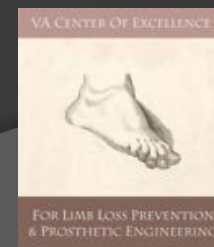
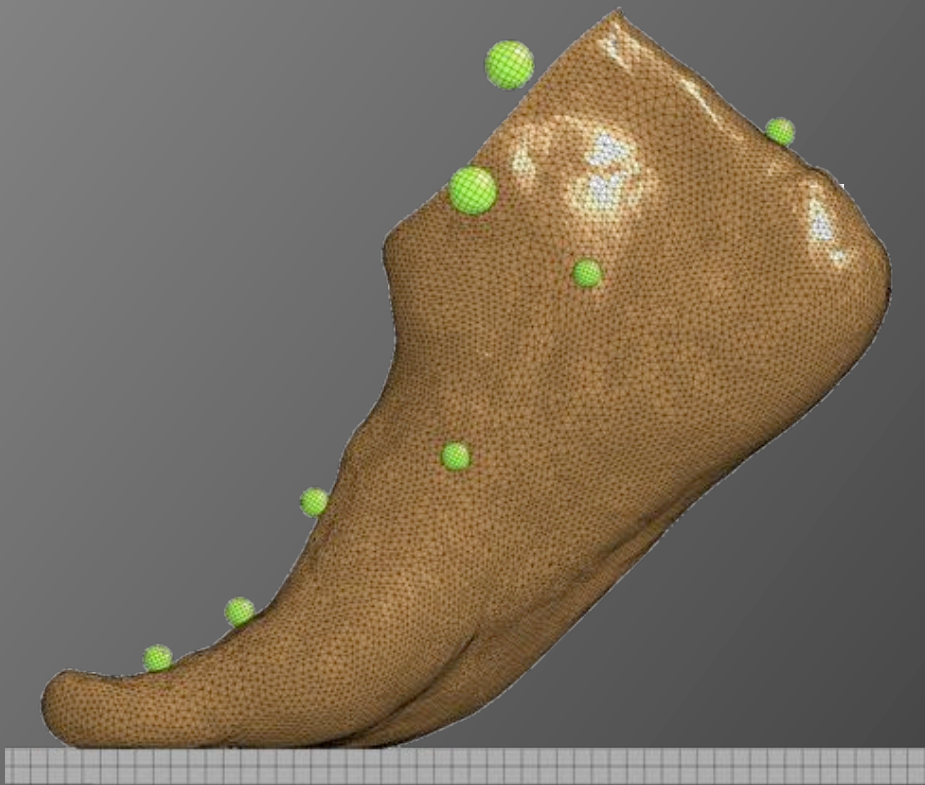


# FINITE ELEMENT MODELING OF THE FOOT

PhD FINAL EXAMINATION  
03/11/2015

**Vara Isvilanonda**



# Objective

*To develop and validate two subject-specific FE foot models (normal and diabetic), to explore the plantar pressure and internal soft tissue stress during quiet stance and the stance phase of gait, and to investigate the effect of soft tissue assumptions.*

# Normal and diabetic subjects

- ⦿ Normal subject

- Age 43 year-old (male)
- Body weight 945 N

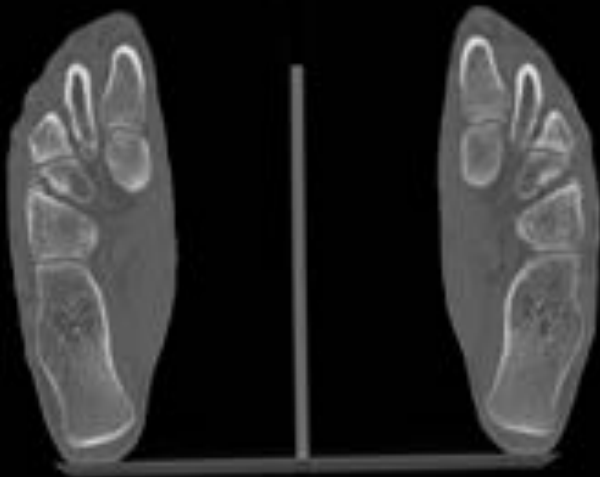
- ⦿ Diabetic subject

- Age 31 year-old (male)
- Body weight 688 N
- Duration of diabetes > 25 years

# FE foot model development

Obtain imaging data

CT (10% BW per foot)



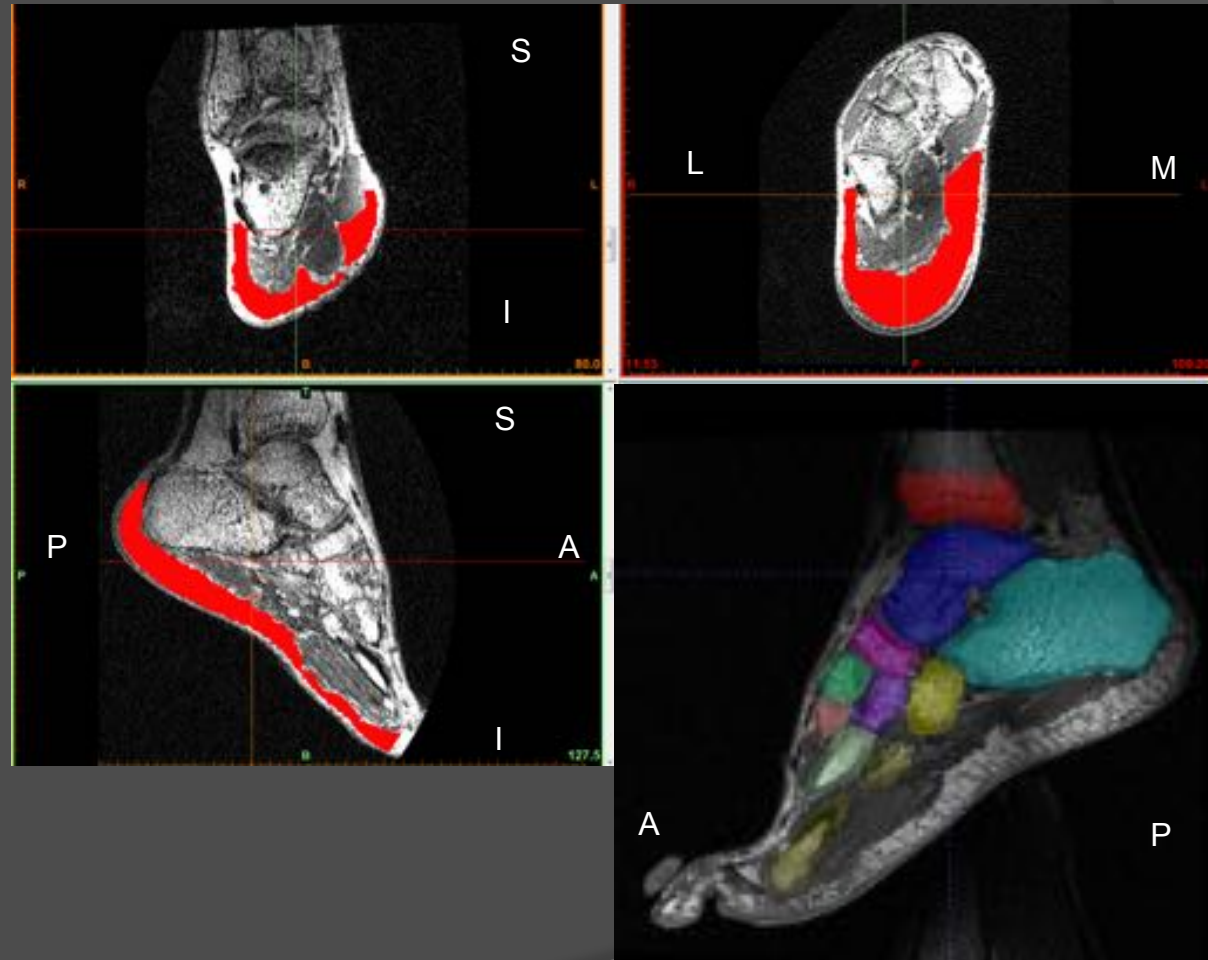
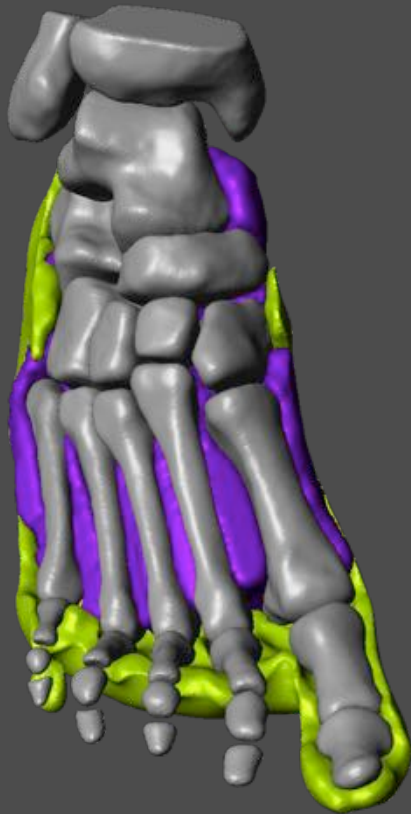
Bone anatomy

MRI (unloaded)



Skin, fat and muscle anatomy

# Segmentation



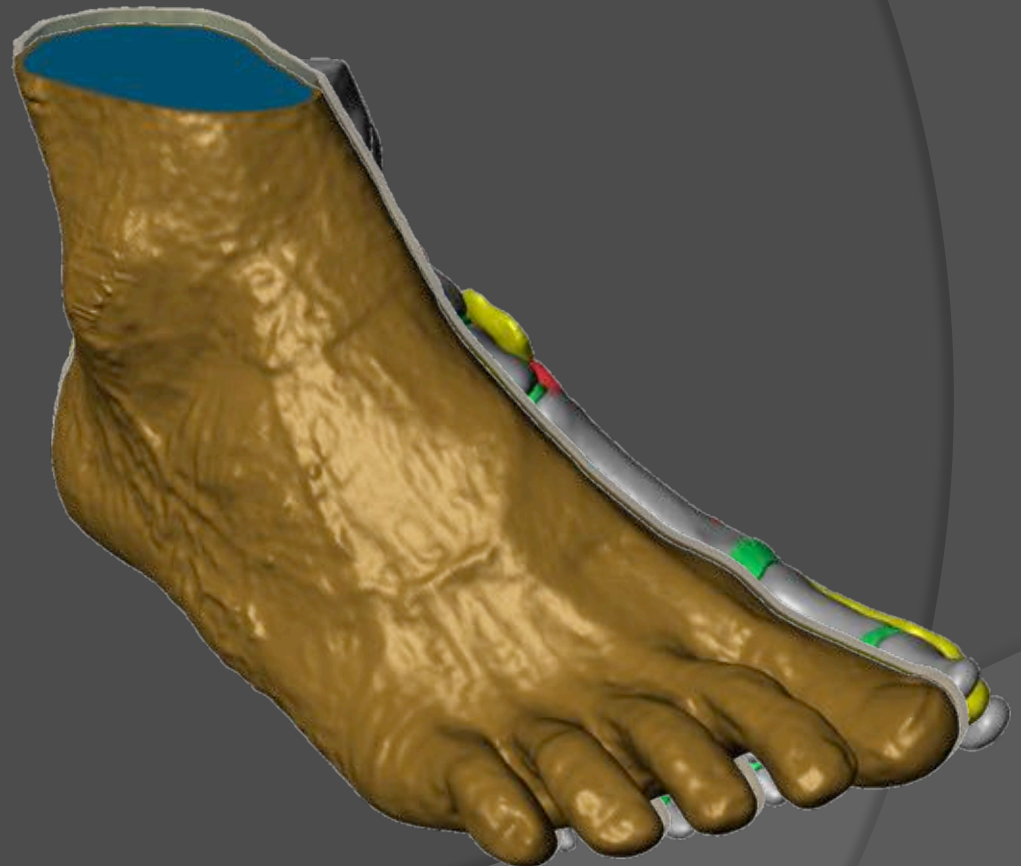
# Boolean operations

Generate joint cavities

Generate skin thickness

Smoothen surfaces

Eliminate gaps/overlaps



# FE model pre-processing

- Mesh with tetrahedral elements
- Element size (2.5mm), type (ELFORM13) determined from mesh convergence analysis
- Bone-soft tissue share nodes





# Material properties

- Materials: rigid bone, Ogden hyperelastic soft tissue

$$W(\lambda_1, \lambda_2, \lambda_3) = \frac{\mu}{\alpha} (\tilde{\lambda}_1^\alpha + \tilde{\lambda}_2^\alpha + \tilde{\lambda}_3^\alpha - 3) + \frac{1}{2} K (J - 1)^2$$

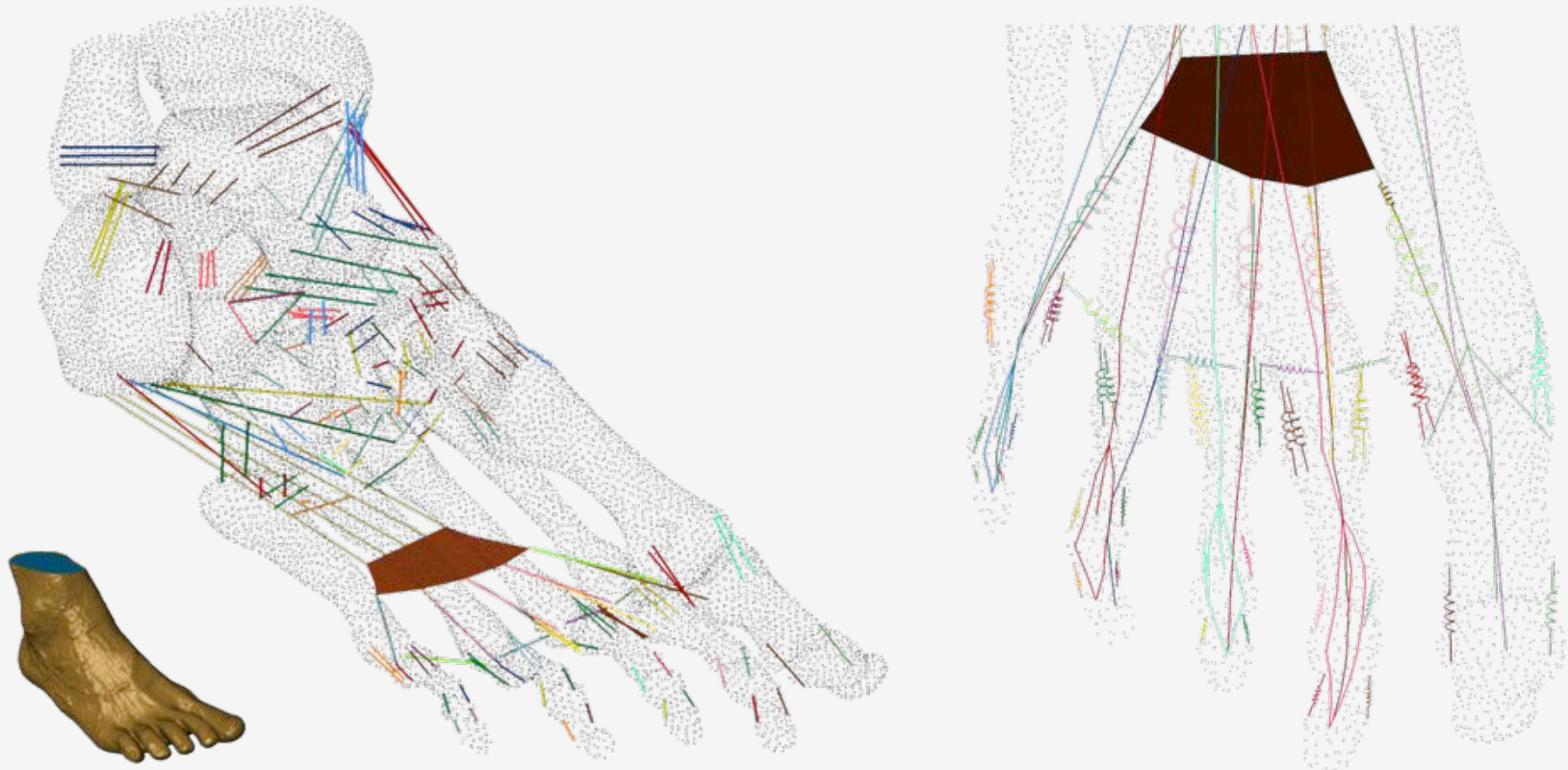
$$\tilde{\lambda}_i = \frac{\lambda_i}{J^{1/3}}$$

- $(\mu_s, \alpha_s)$ ,  $(\mu_F, \alpha_F)$  and  $(\mu_M, \alpha_M)$  are subject-specific skin, fat and muscle material properties **determined *in vivo* (Specific Aim 2)**
- Dorsal soft tissue modeled with subject-specific generic soft tissue  $(\mu_G, \alpha_G)$



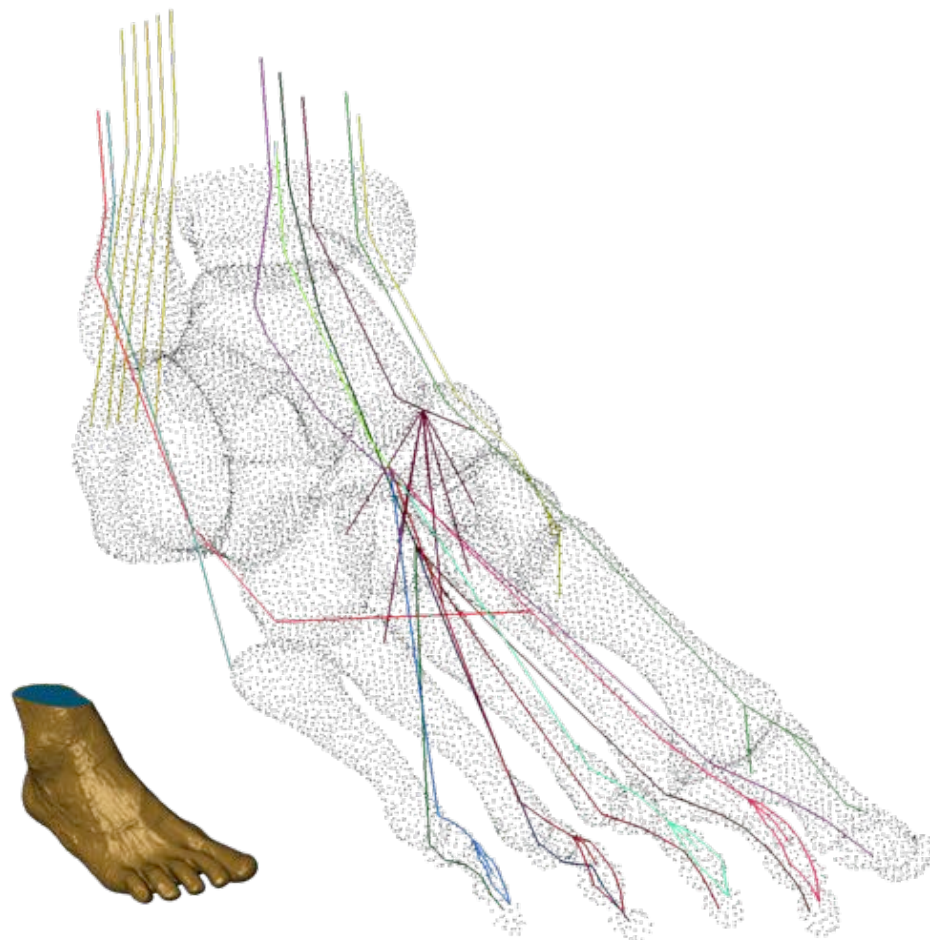
# Ligament

- 102 non-linear, tension only ligaments



# Tendon

- 9 extrinsic muscle tendons (seatbelts – slip rings)

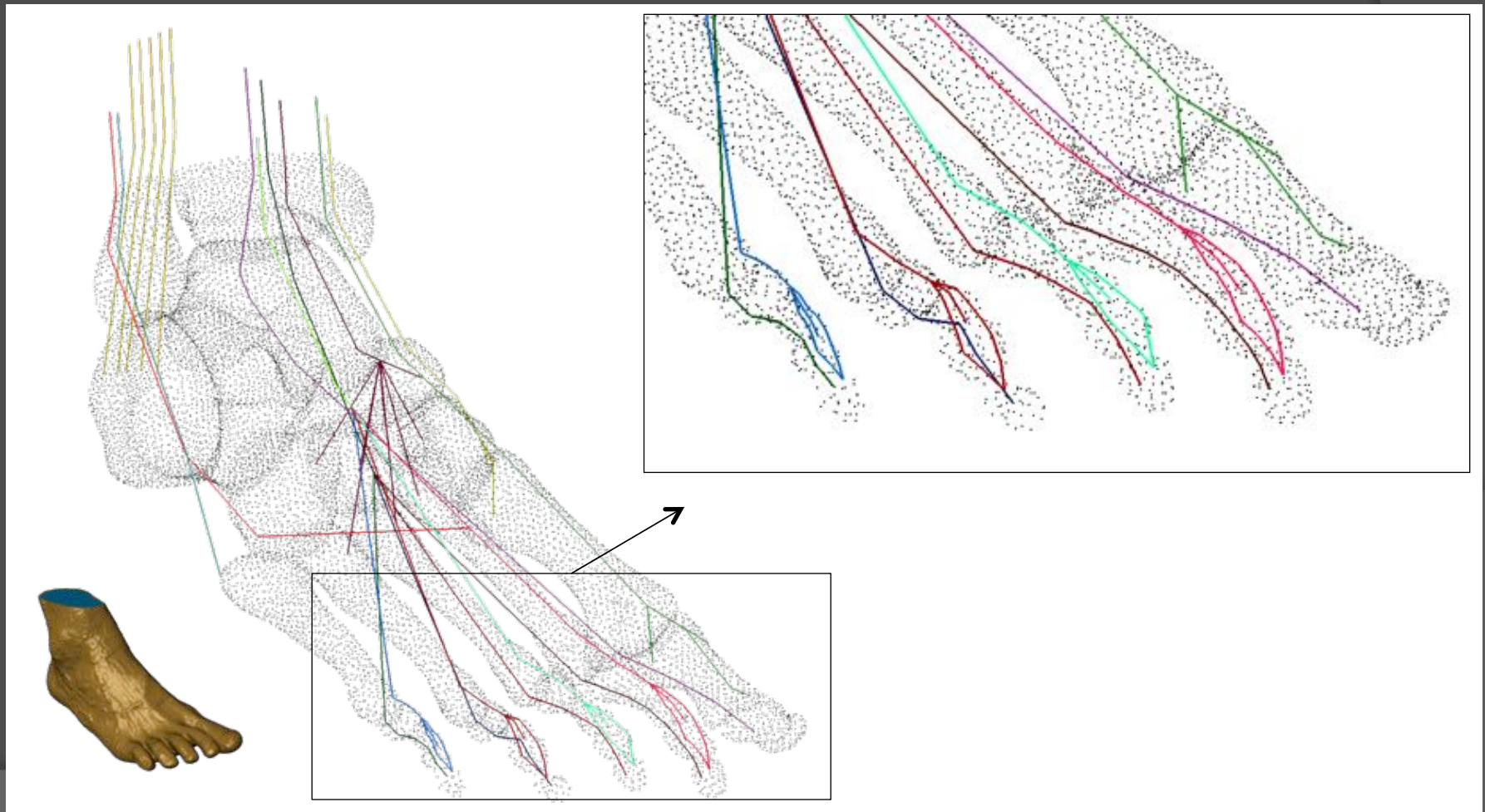


9 Tendons are:

- Achilles
- Tibialis anterior
- Tibialis posterior
- Peroneus longus
- Peroneus brevis
- Extensor hallucis longus
- Extensor digitorum longus
- Flexor hallucis longus
- Flexor digitorum longus

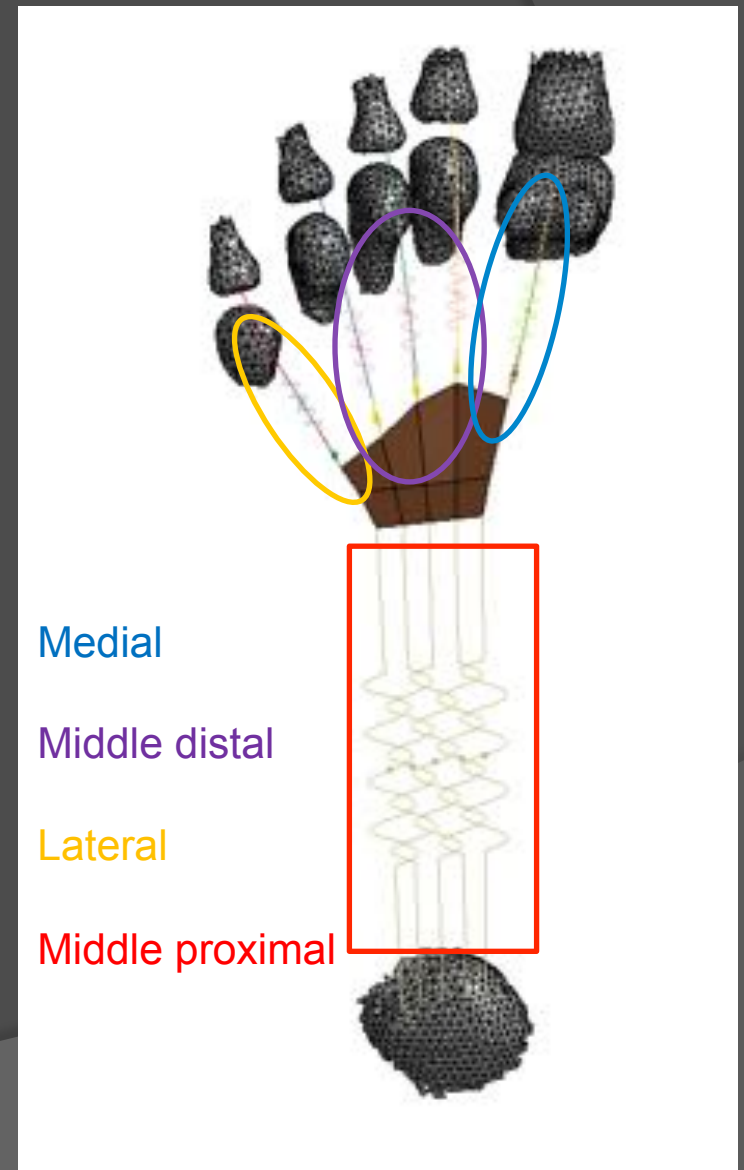
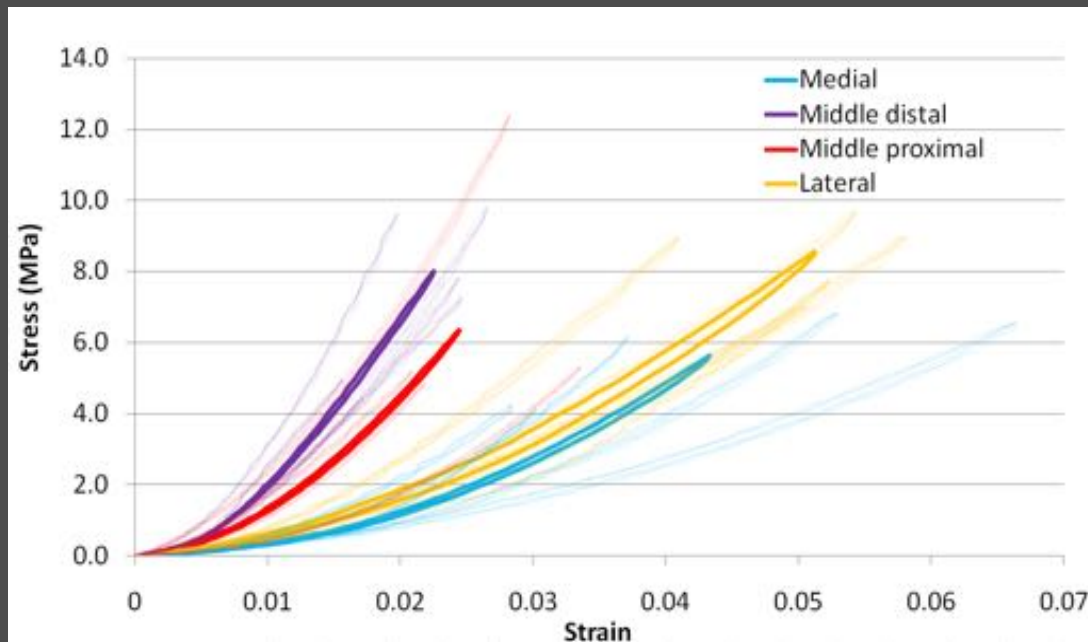
# Tendon

- 9 extrinsic muscle tendons (seatbelts – slip rings)

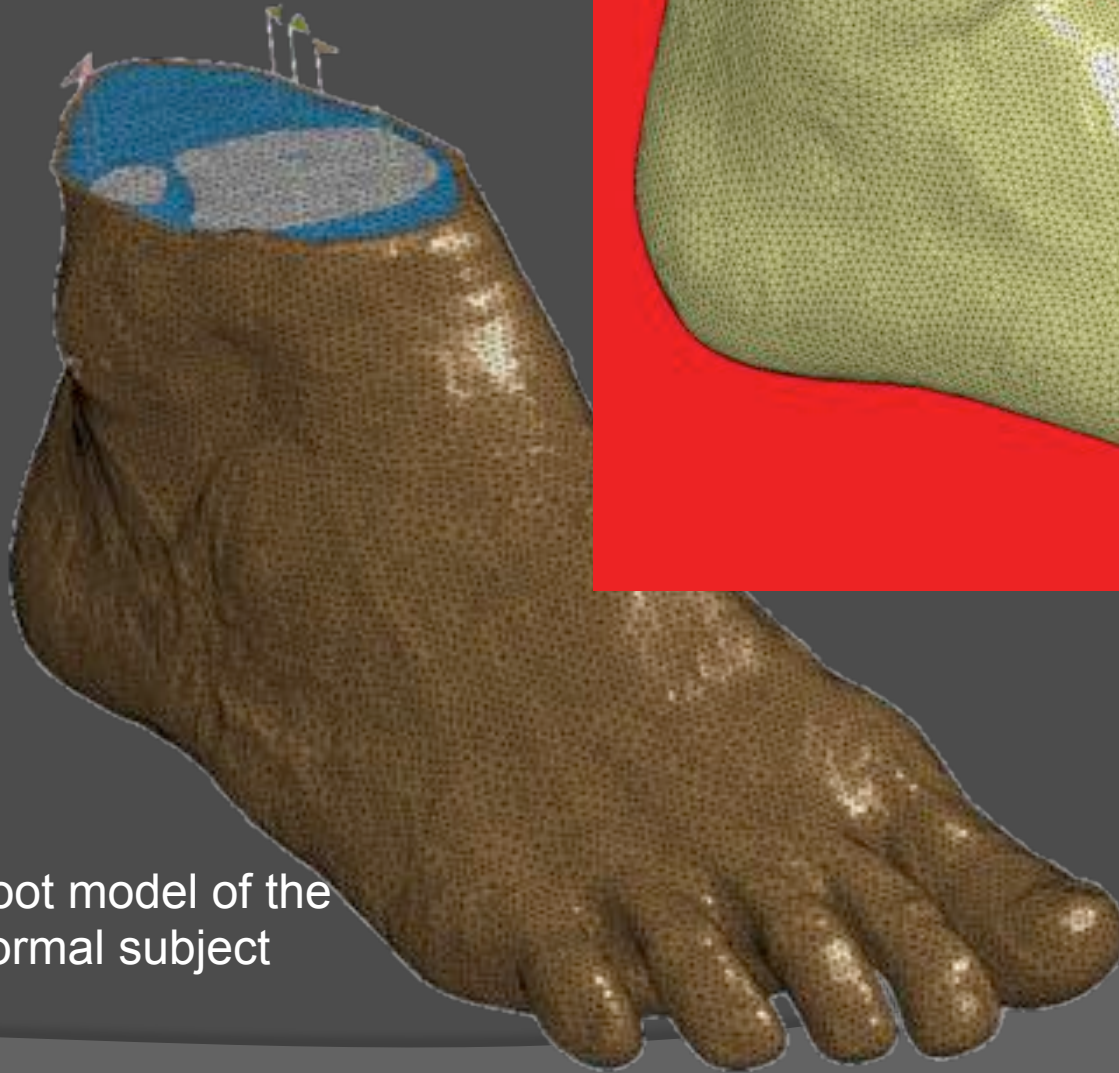


# Plantar fascia

- Material properties in 4 regions from cadaveric tests from 3<sup>rd</sup> Specific Aim







Foot model of the  
normal subject



Foot model of the  
diabetic subject

# Experimental Validation

3 validation conditions

- ⦿ Quasi static: Passive 10% BW foot compression
- ⦿ Quasi static: Quiet stance
- ⦿ Dynamic: Stance phase of gait

# Validation 1: passive compression

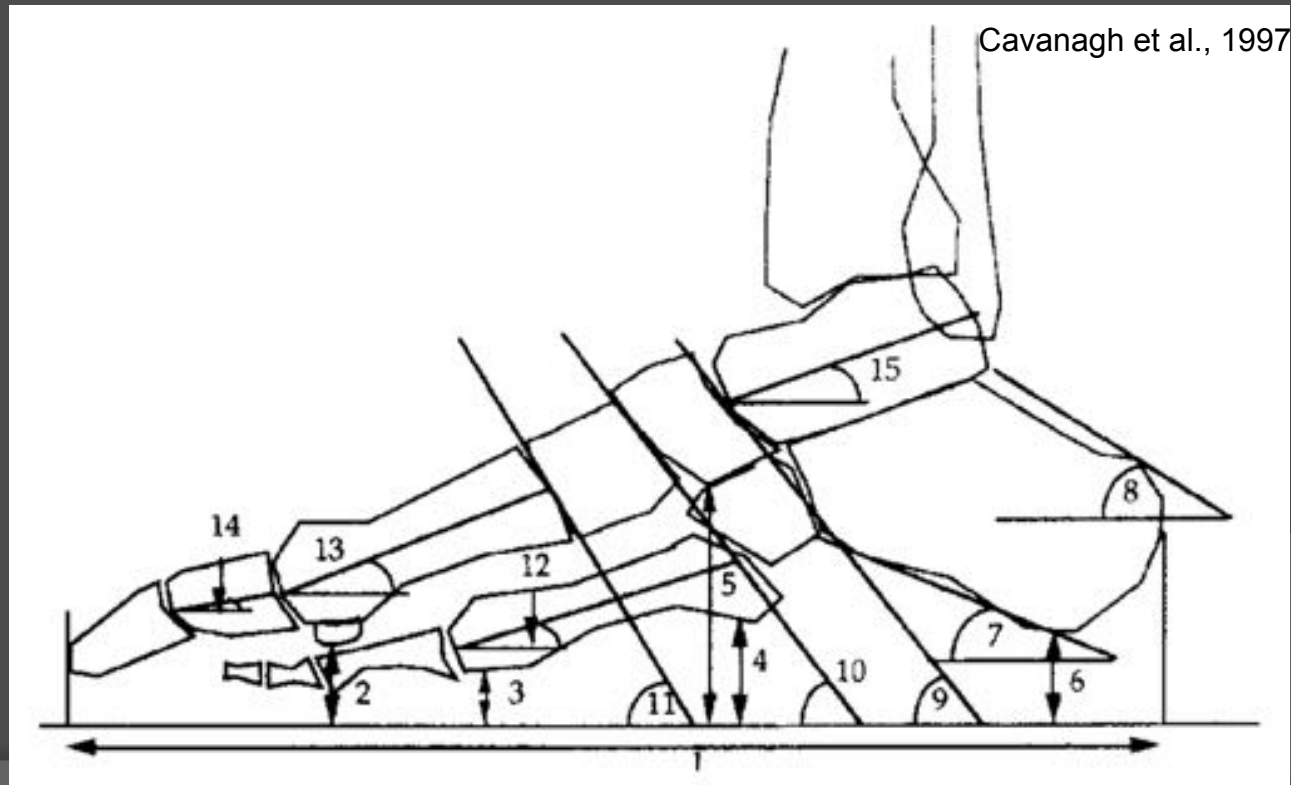
- Bony alignments from 10% BW CT data are compared to simulation



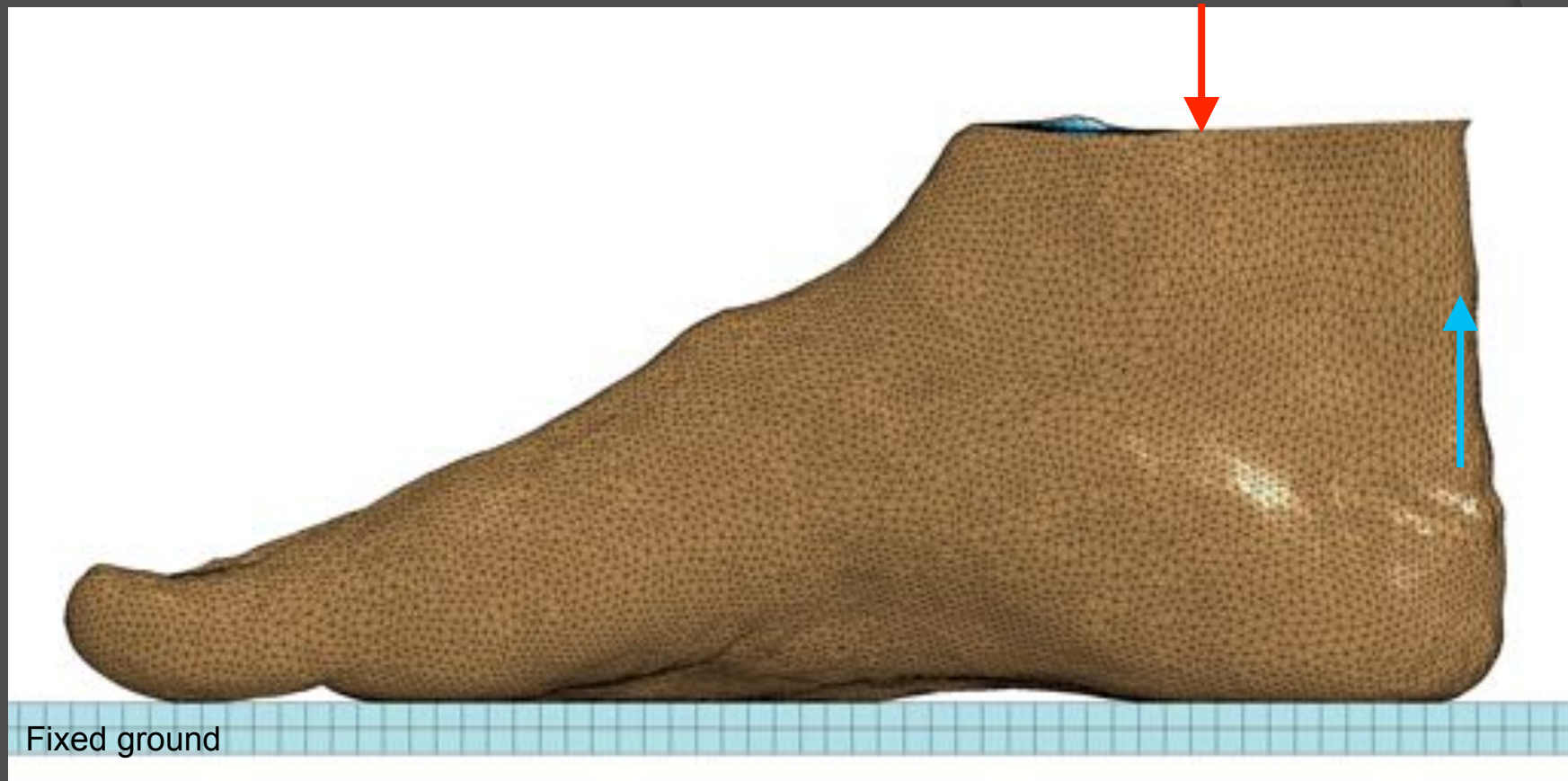


# Validation 1: passive compression

- Bony alignments from 10% BW CT data are compared to simulation

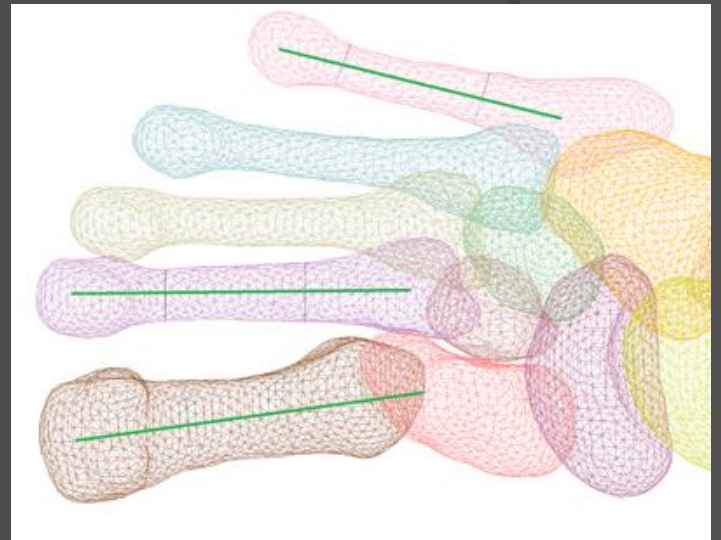
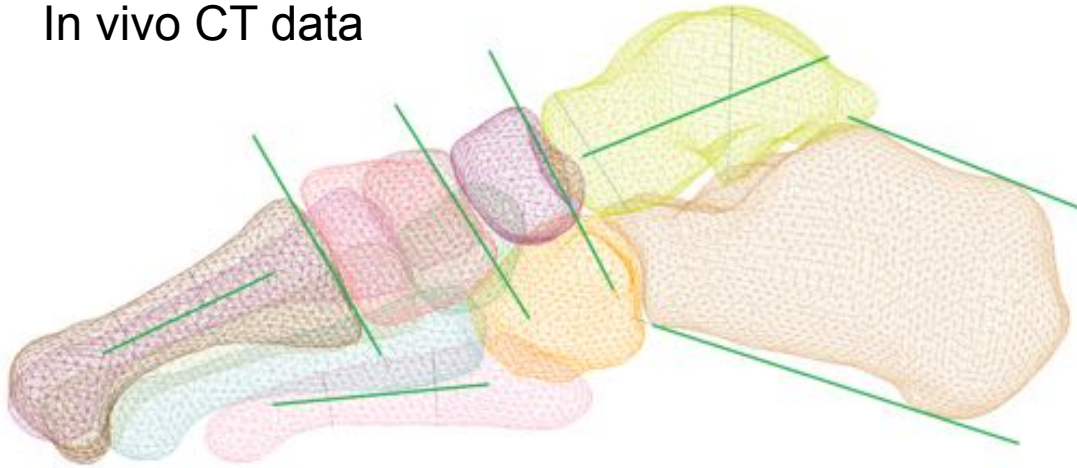


# Passive compression FE simulation

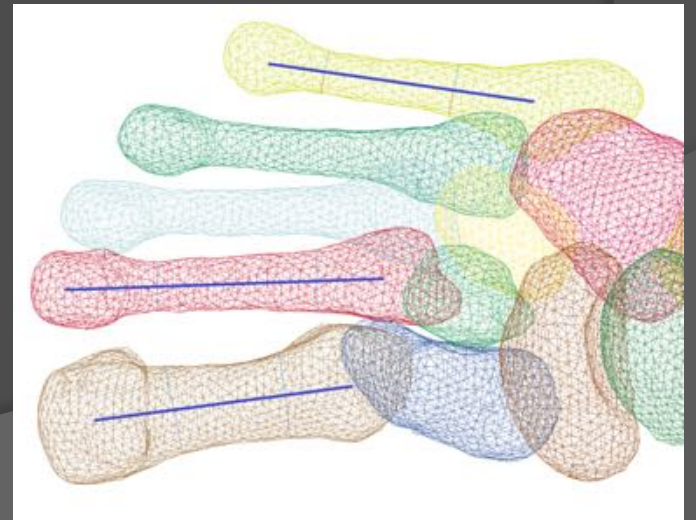
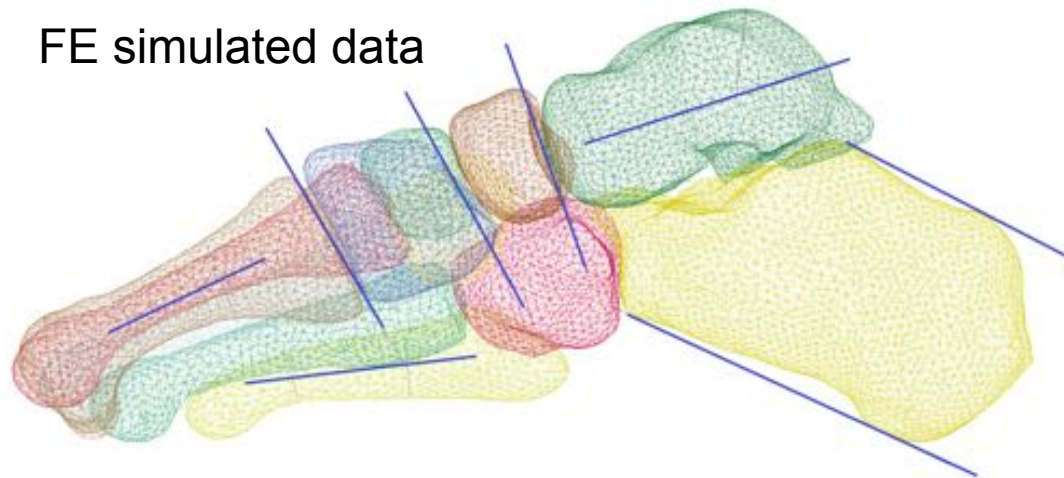


# Passive compression FE simulation

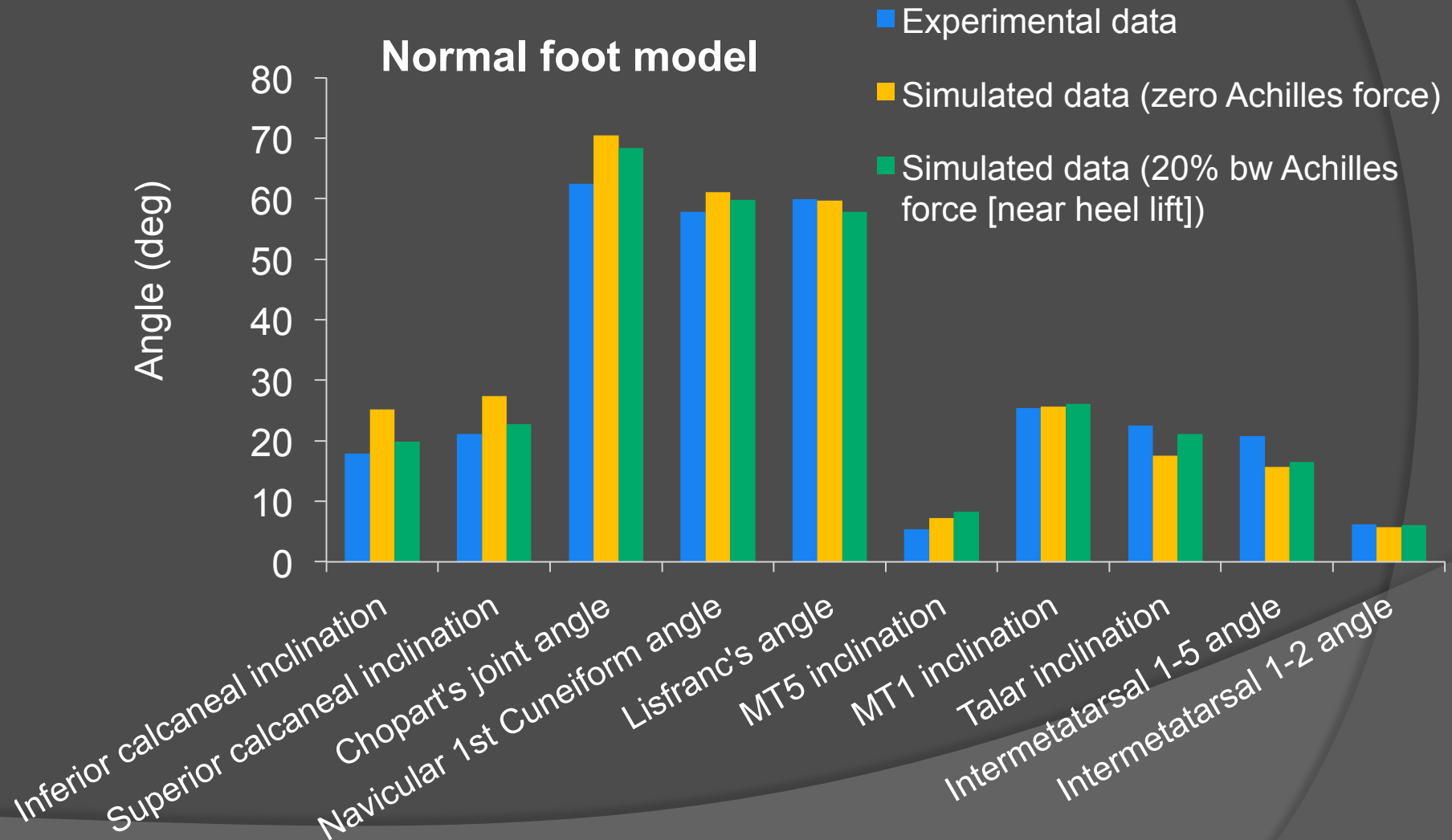
In vivo CT data



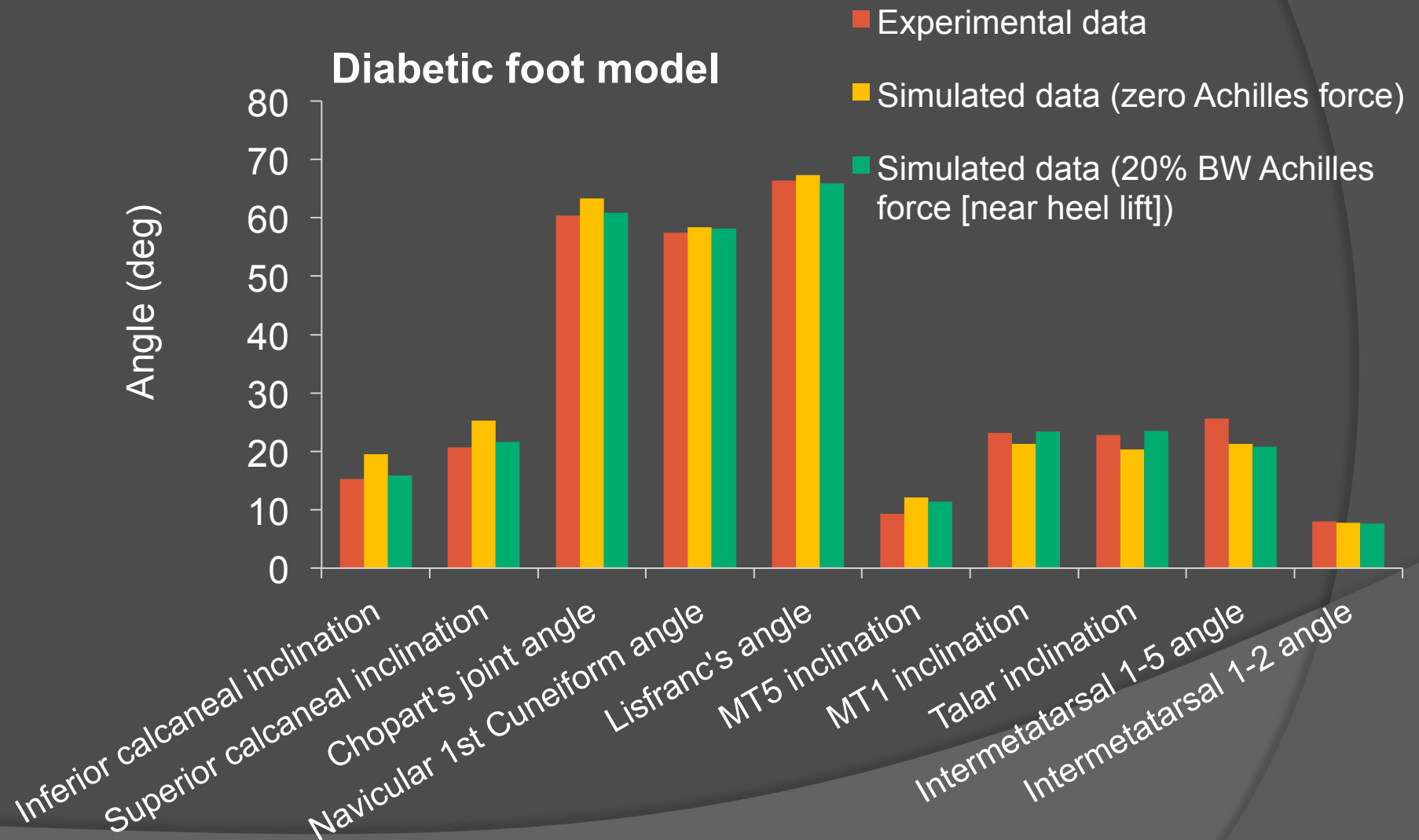
FE simulated data



# Passive compression validation results



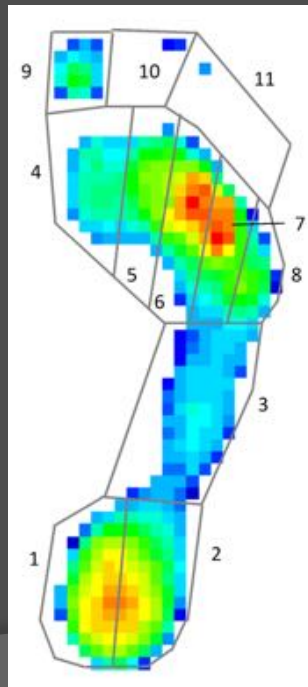
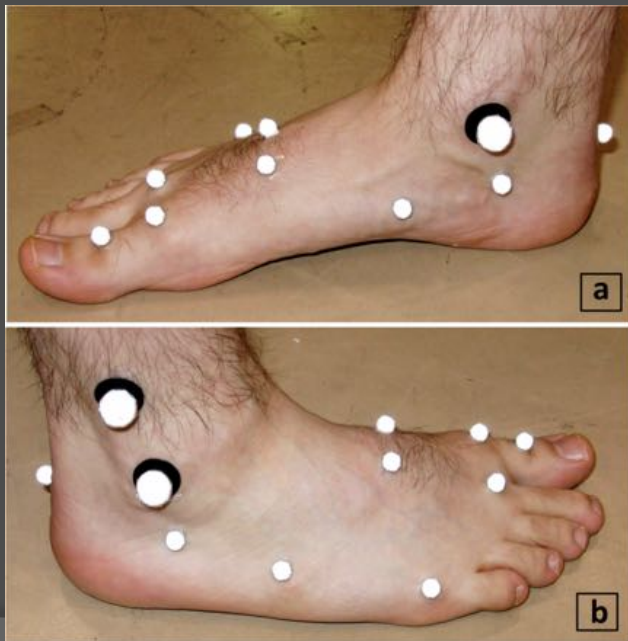
# Passive compression validation results





## Validation 2: Quiet stance

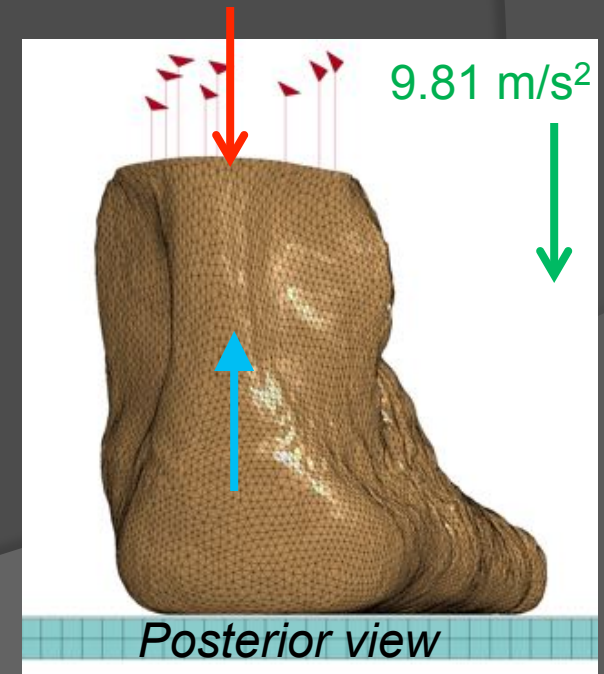
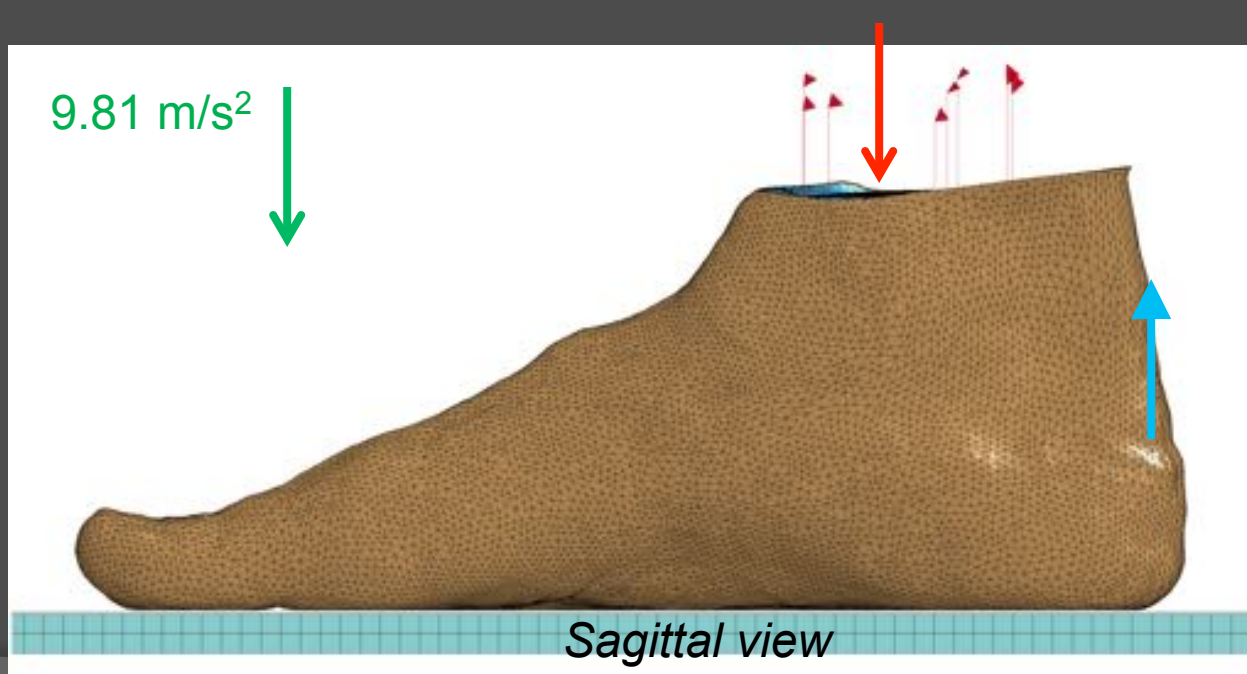
- Recorded 14 foot retro-reflective markers<sup>1</sup> using 12-camera Vicon system
- Recorded plantar pressure on an emed-x pressure platform



<sup>1</sup> [Leardini et al., *Gait & Posture*, 25: 453-462

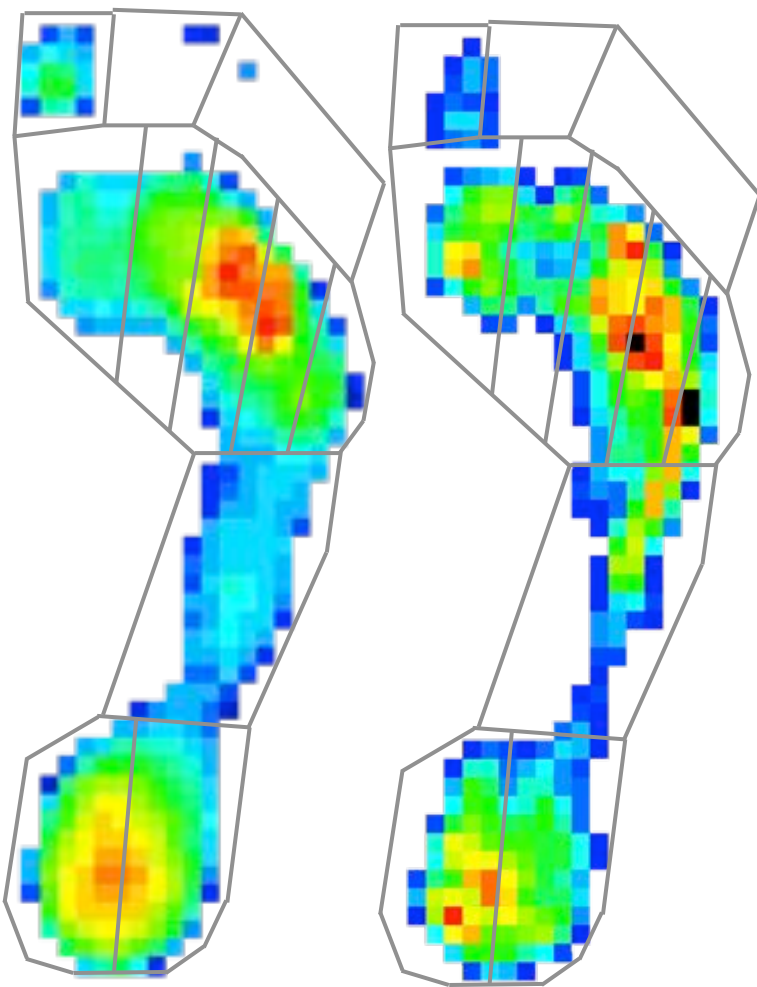
# Quiet stance FE simulation

- Prescribed tibia orientation from motion capture data
- **Tibial force** + **Achilles tendon force** + **gravitational force** = **50% BW**
- Tune Achilles tendon force to match *in vivo* COP location





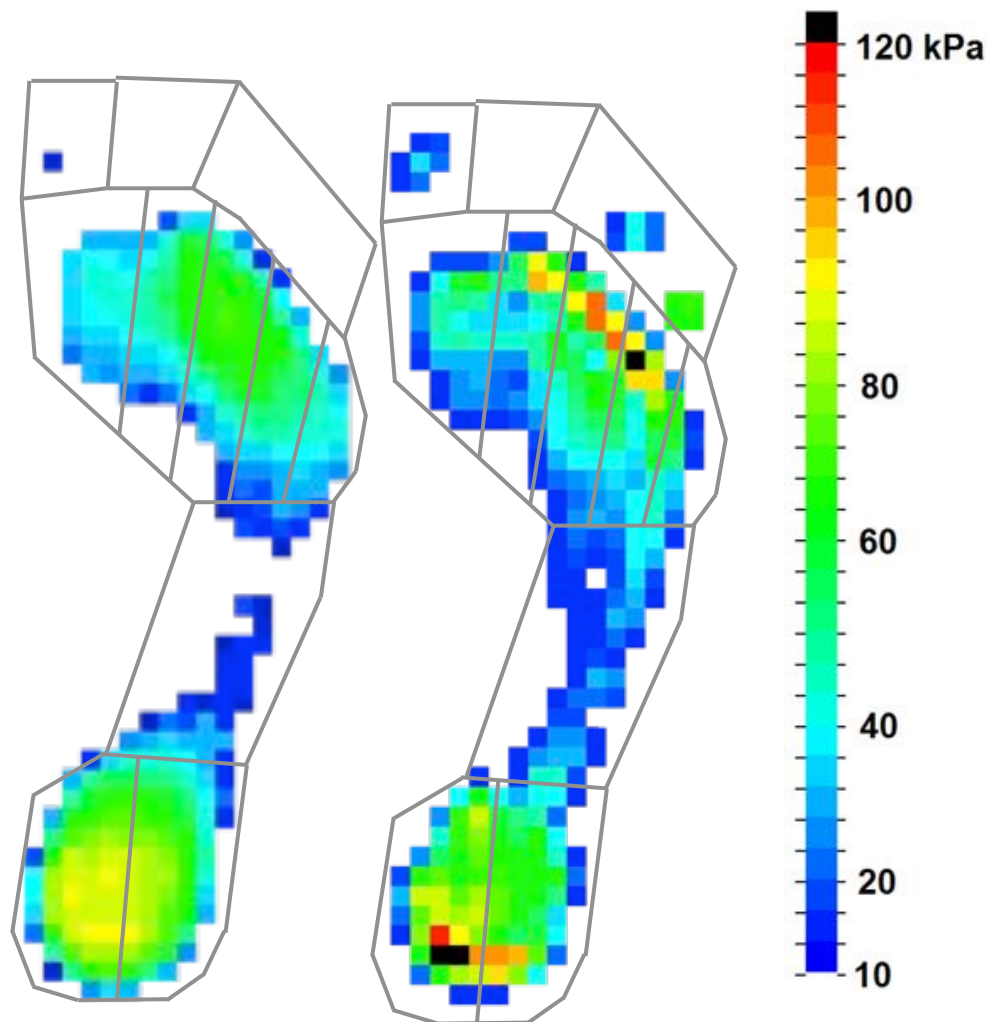
## Normal



Experimental data

Simulated data

## Diabetic

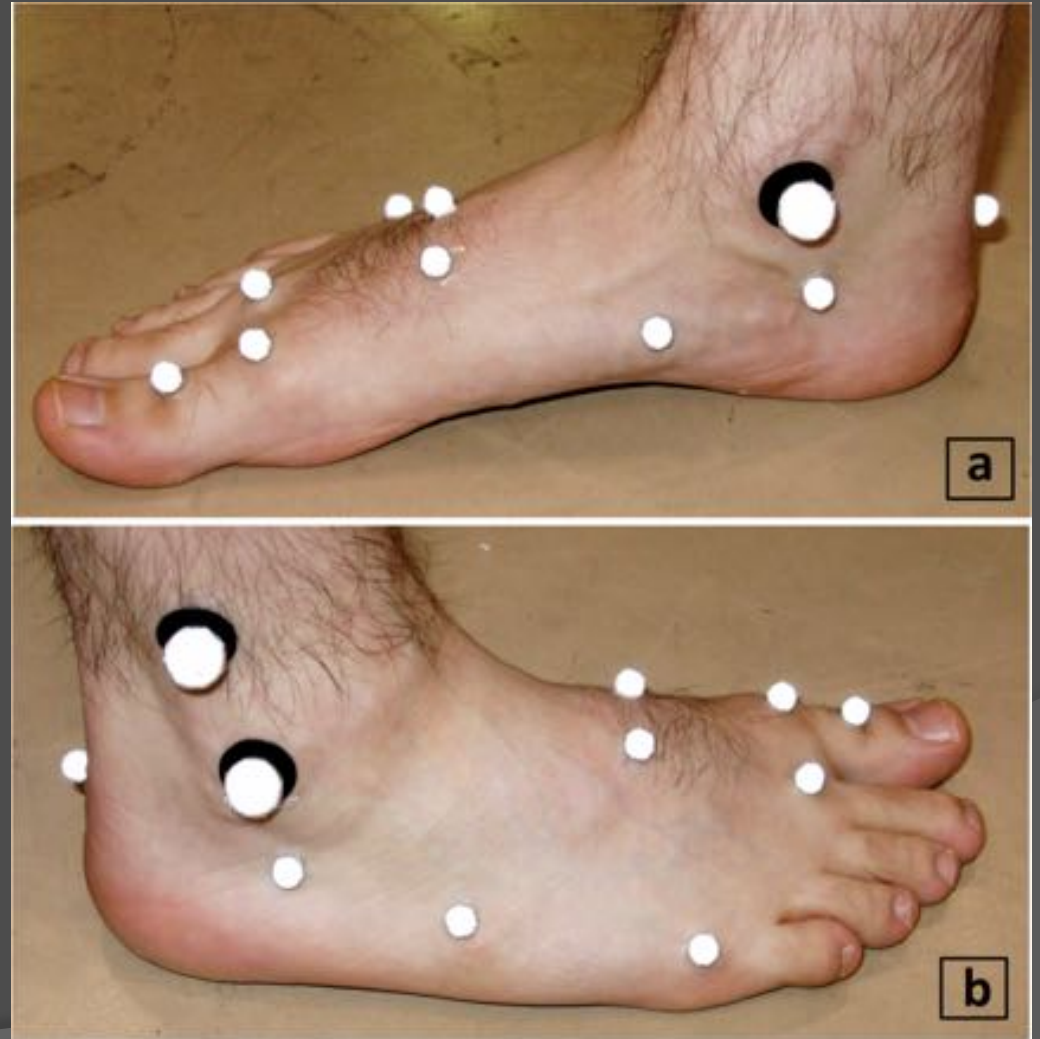


Experimental data

Simulated data

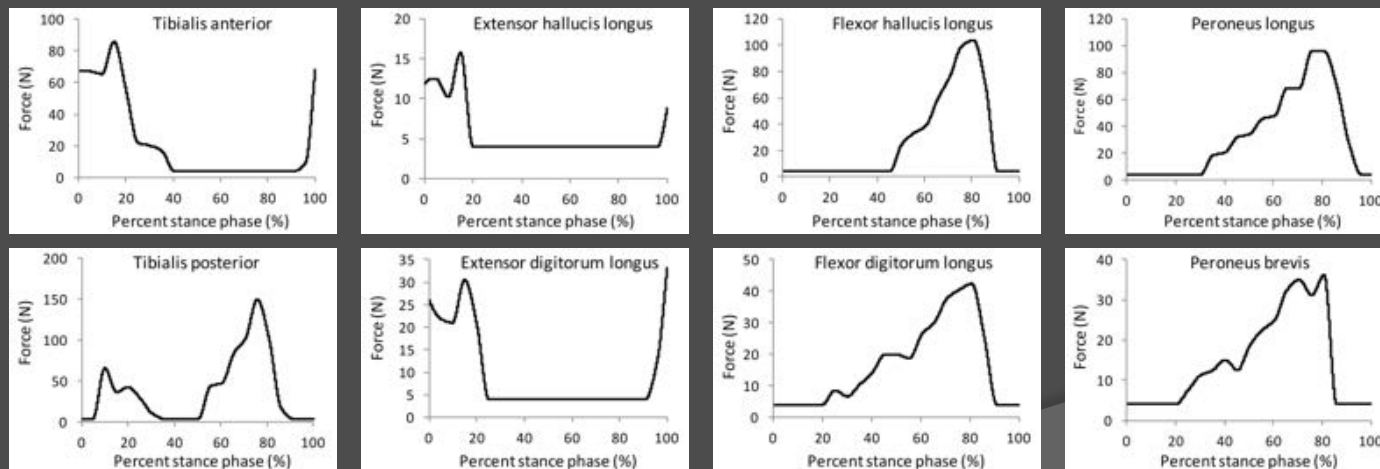
# Validation 3: Dynamic gait

- Self-selected speed
- Right foot strike
- 7 force plate trials
- 7 pressure platform trials



# Gait FE simulation

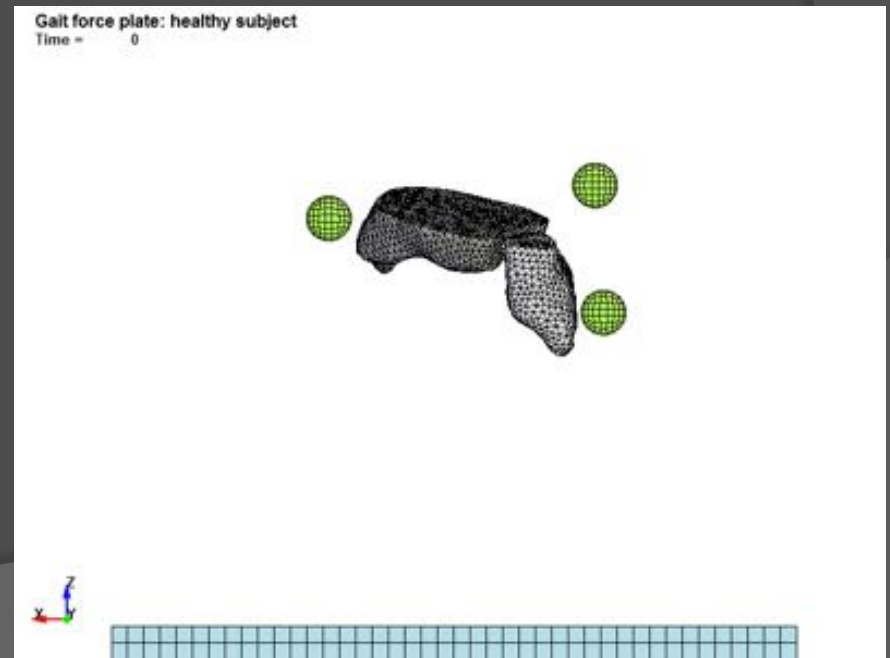
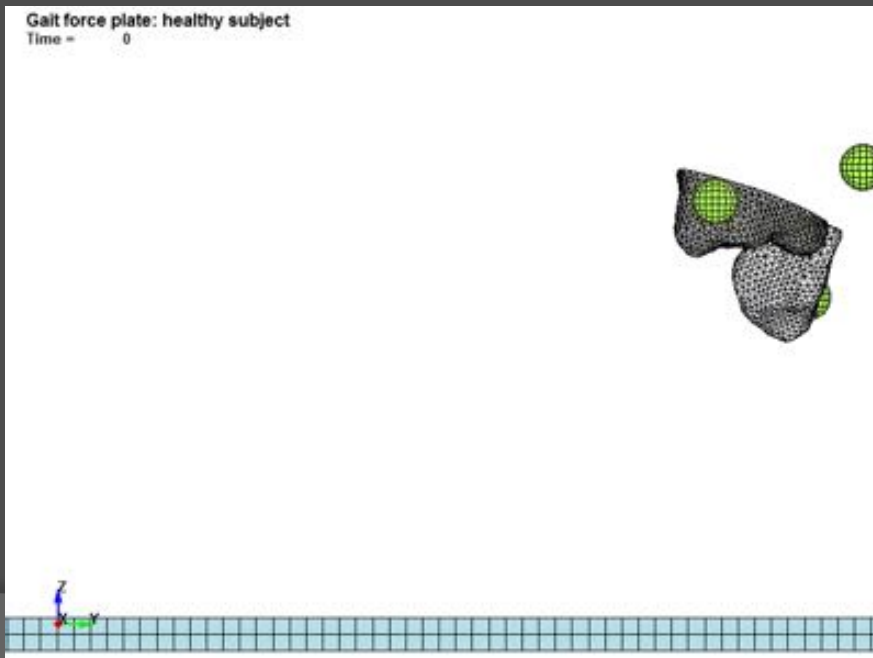
- Different simulation for force plate and pressure platform trials
- Prescribe tibial kinematics-time history (series of 4x4 transformation matrices)
- Prescribe tendon force-time history from literature <sup>1</sup>



<sup>1</sup> [Aubin et al., 2012, *IEEE T. Robot*, **28**: 246-255]

# Gait FE simulation

- ⦿ Different simulation for force plate and pressure platform trials
- ⦿ Prescribe tibial kinematics-time history (series of 4x4 transformation matrices)
- ⦿ Prescribe tendon force-time history from literature <sup>1</sup>

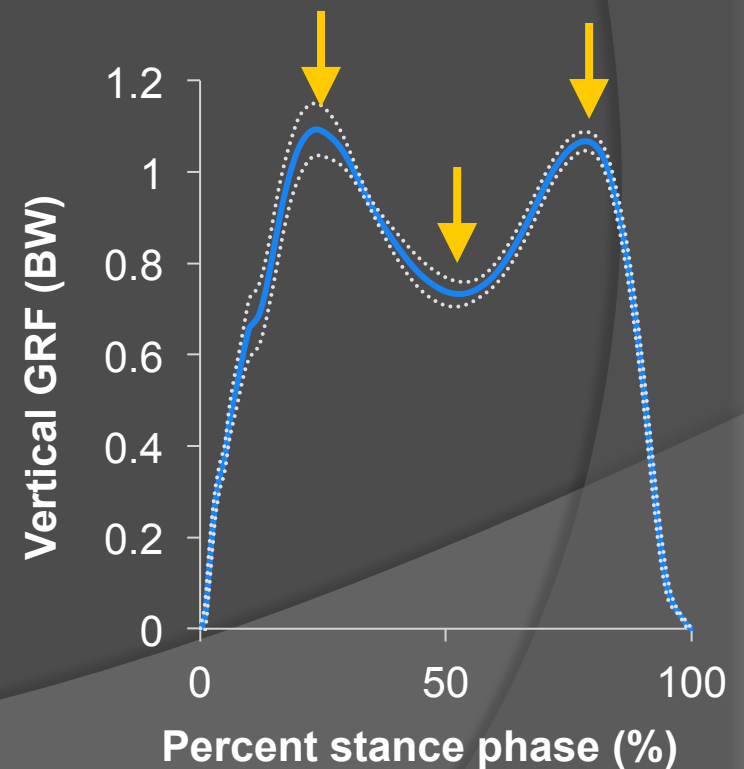


# Gait FE simulation: protocol

- Initialize tendon forces, dorsiflex ankle before heel strike (0.0s to 0.2s)
- At 0.2s, switched to prescribed tibial kinematics
- Stance phase of gait ~0.215s to push off

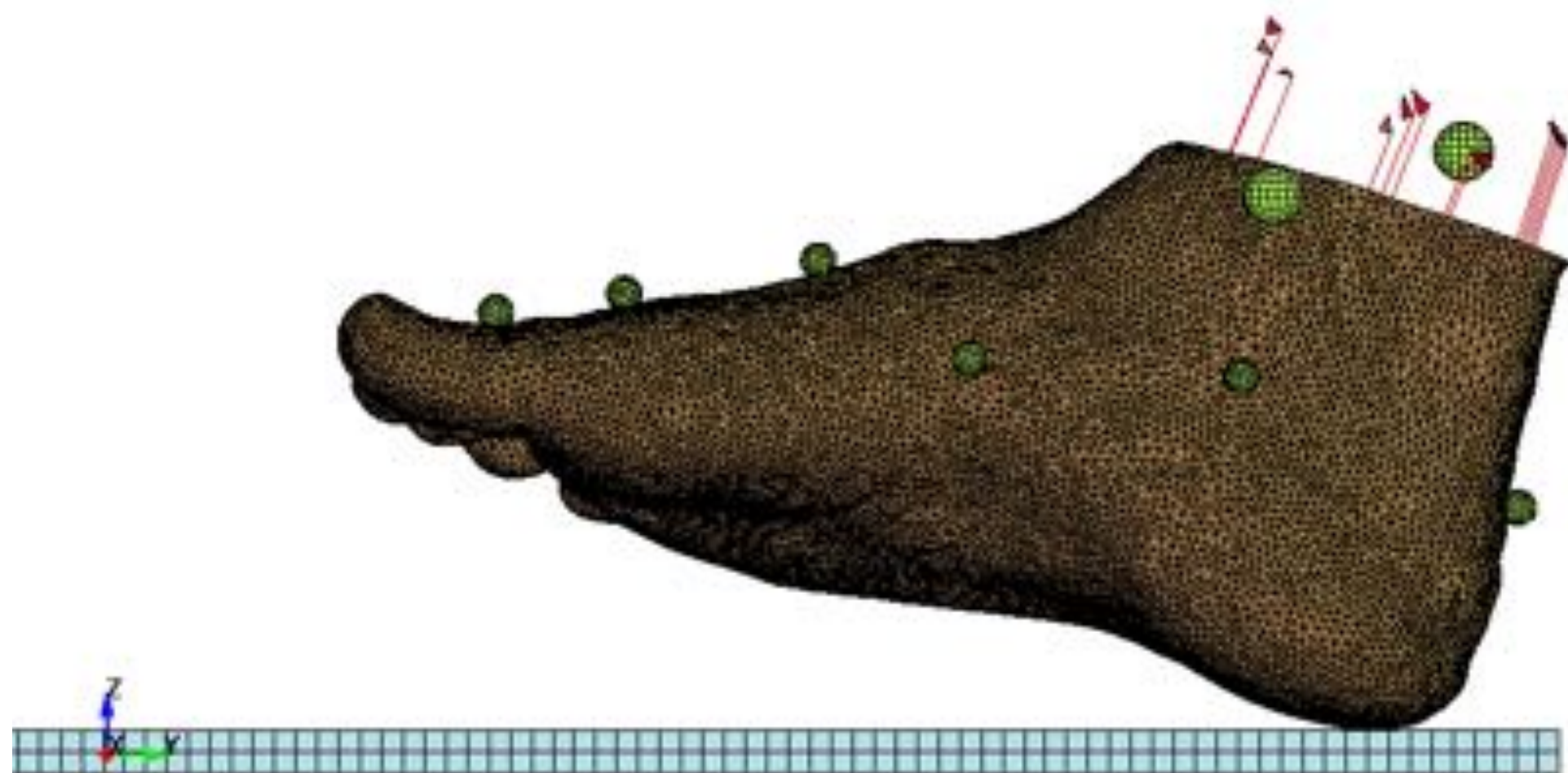
Model tuning to achieve target vertical GRF

- Floor position (1-7mm)
- Achilles tendon force



Gait force plate: healthy subject

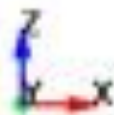
Time = 0





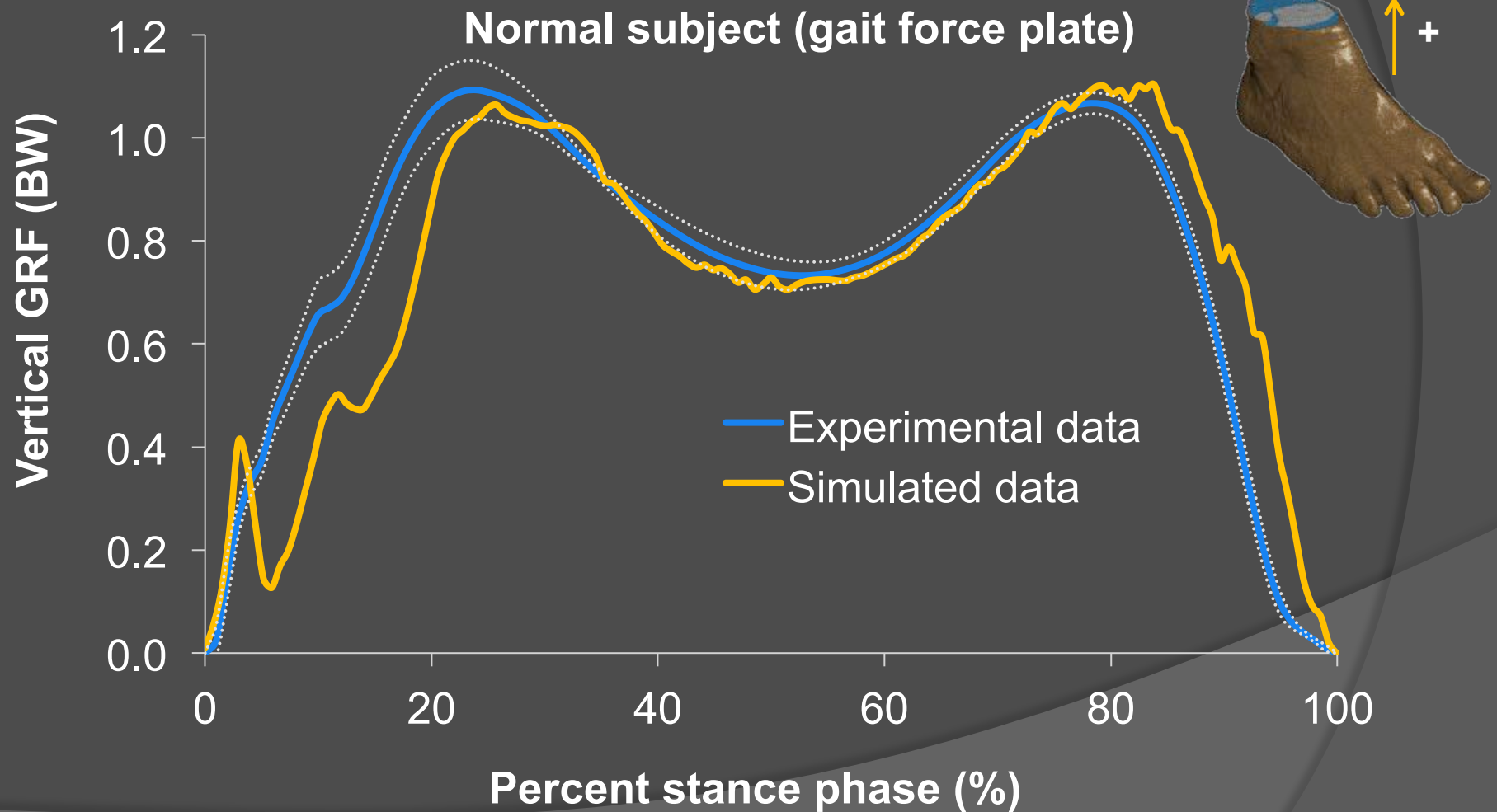
Gait force plate: healthy subject

Time = 0

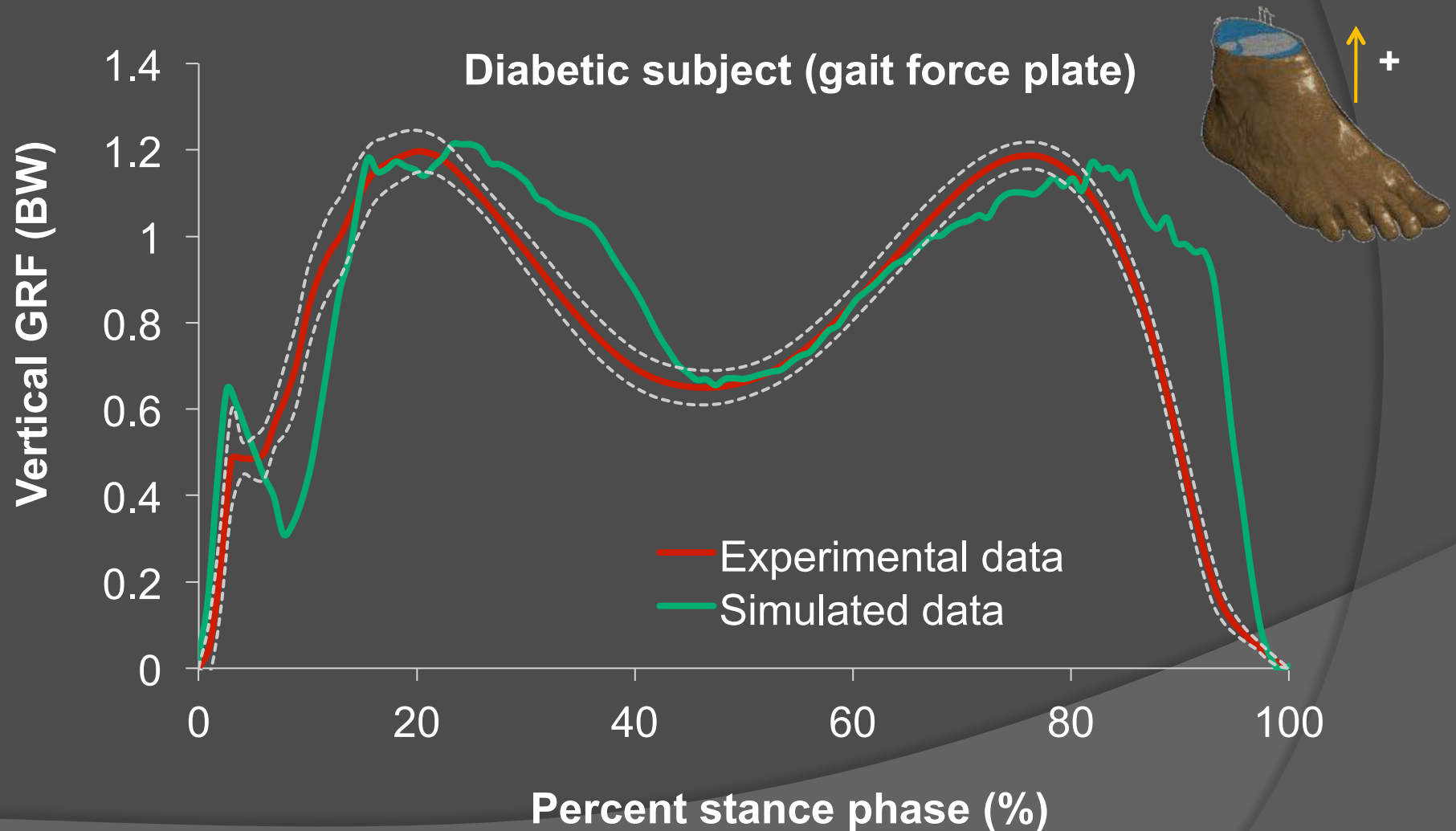




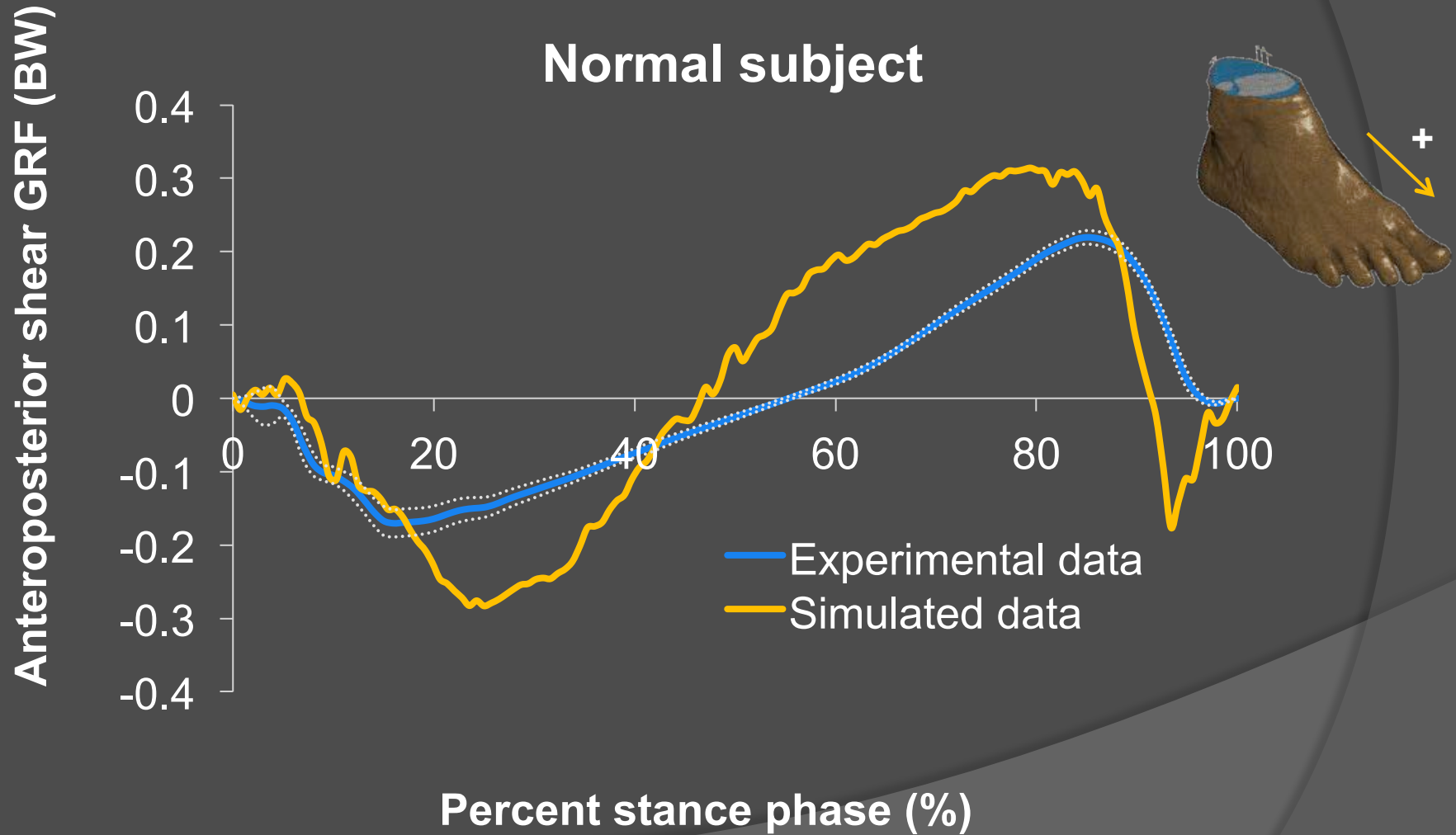
# Gait: Vertical ground reaction force



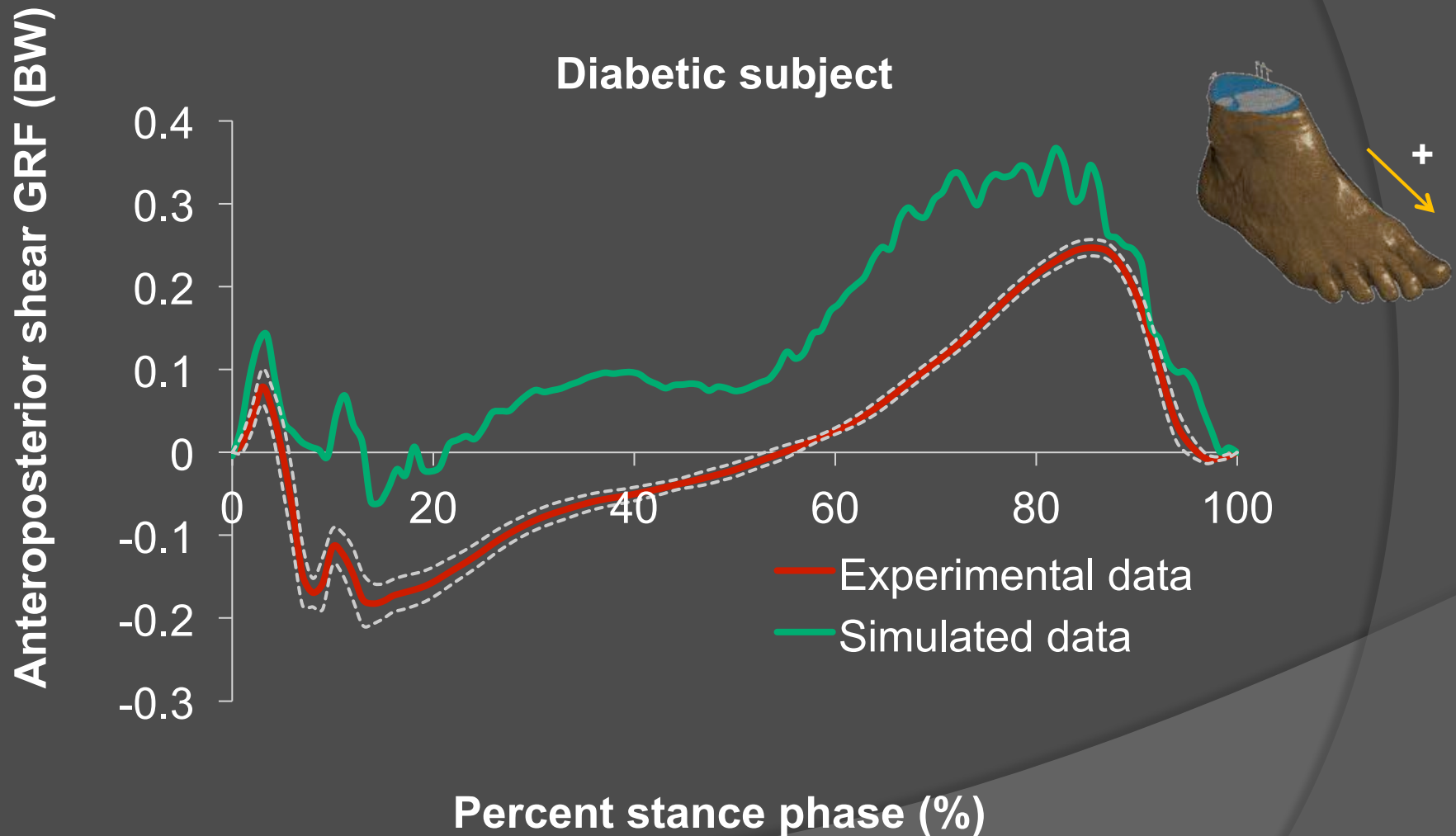
# Gait: Vertical ground reaction force



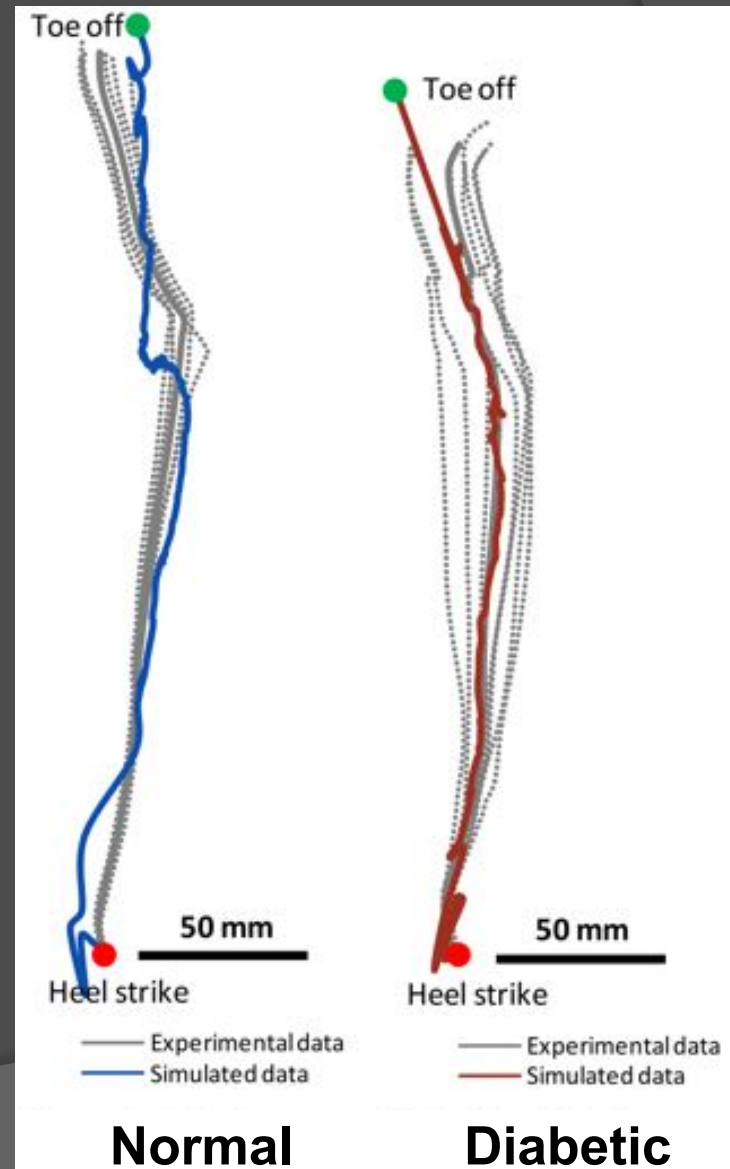
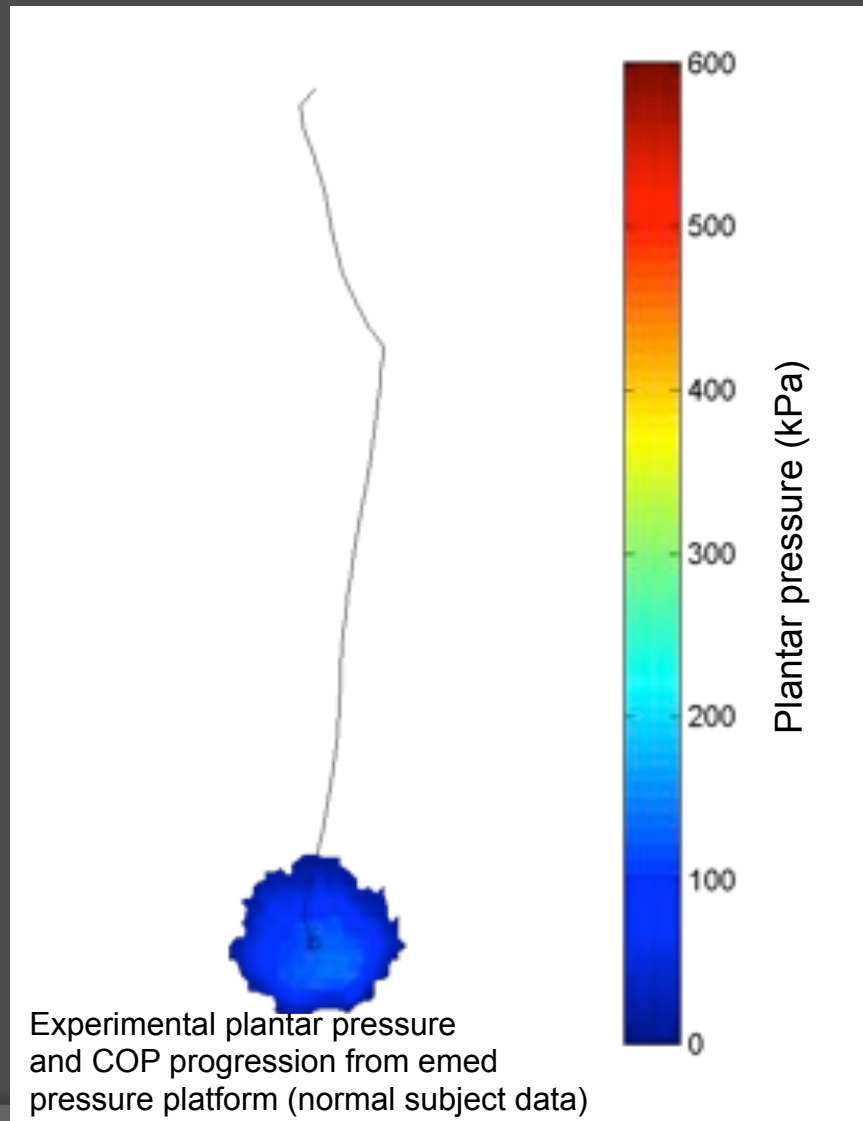
# Gait: AP shear ground reaction force



# Gait: AP shear ground reaction force

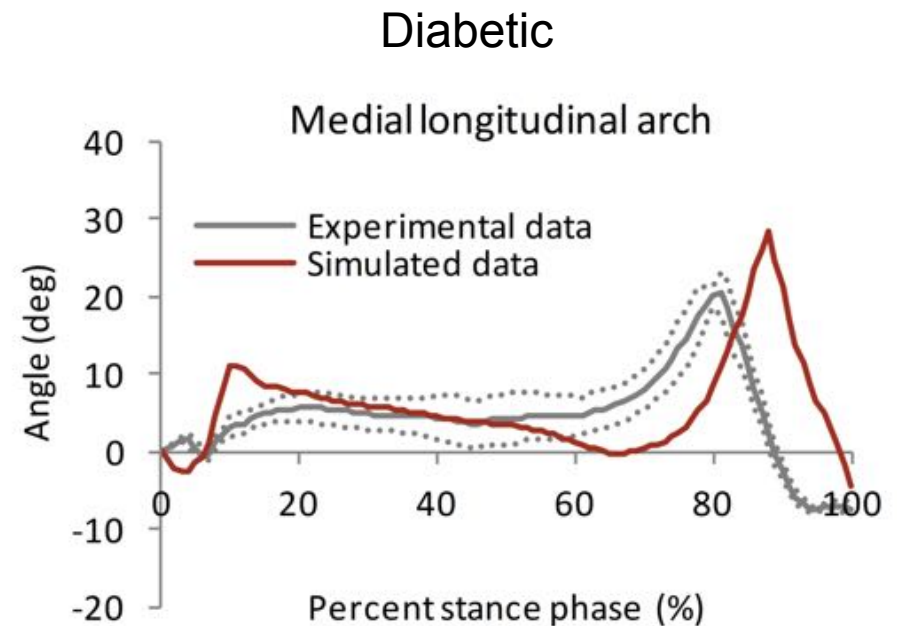
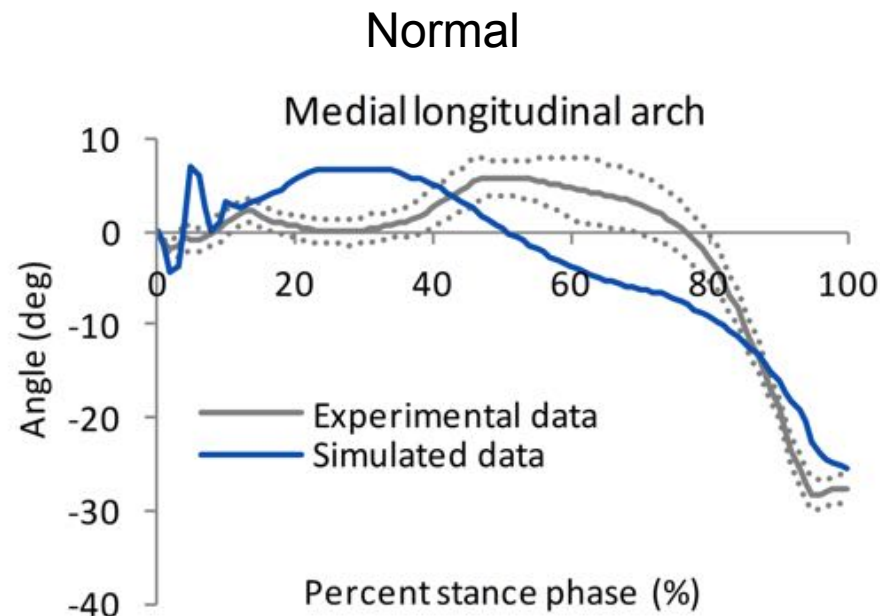


# Gait: Center of pressure



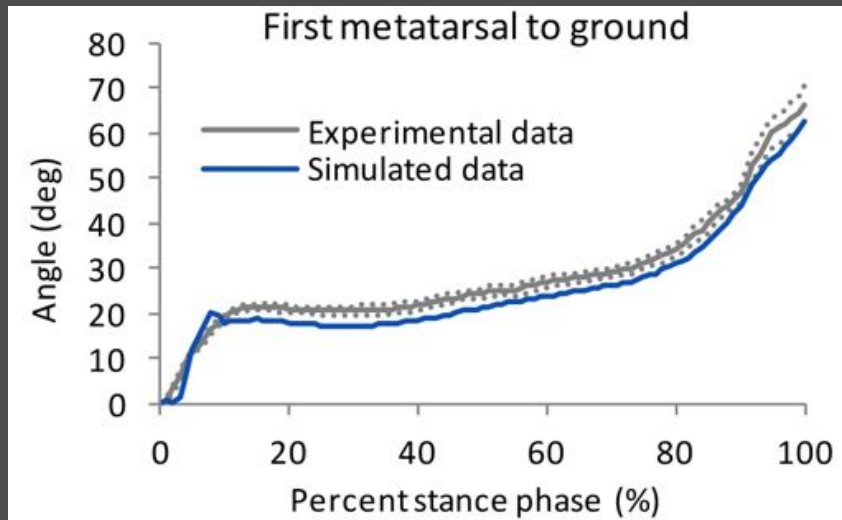
# Gait: Bone kinematics

- Measurements are based on foot model described by Leardini et al., 2007
- 10 bone angle validations showed small RMS error relative to peak

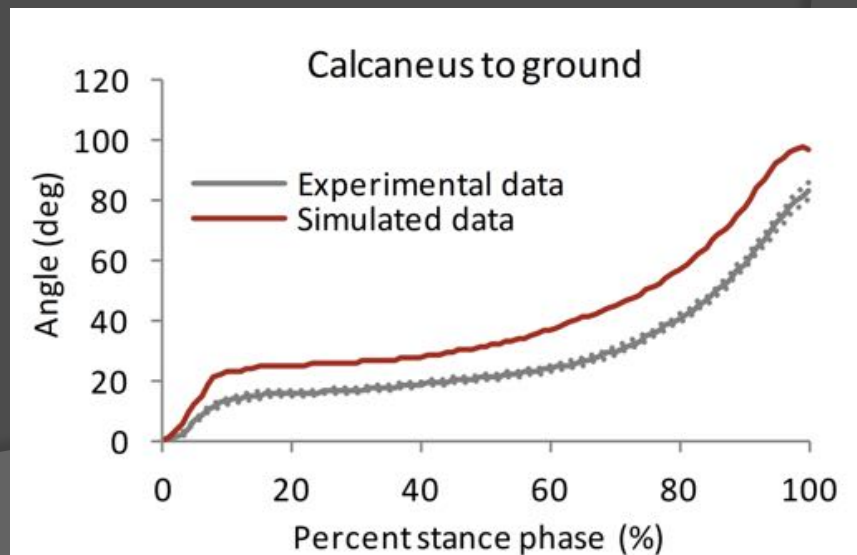
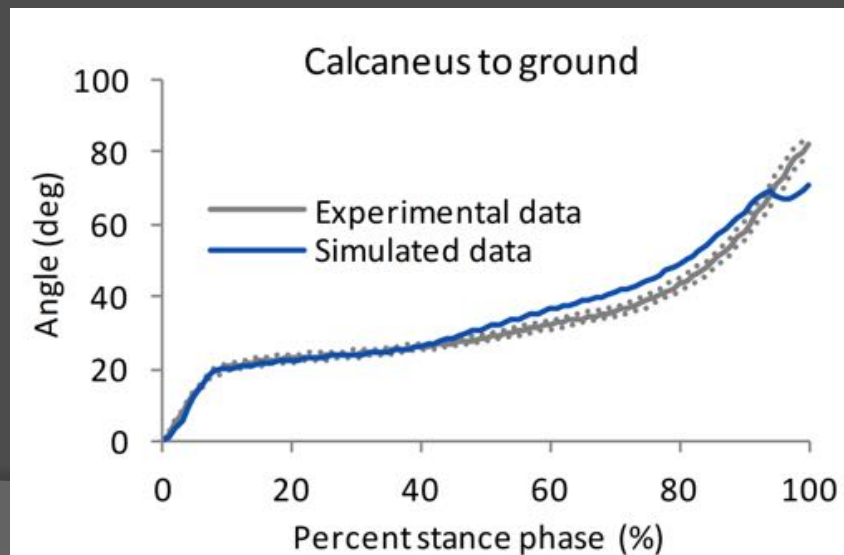
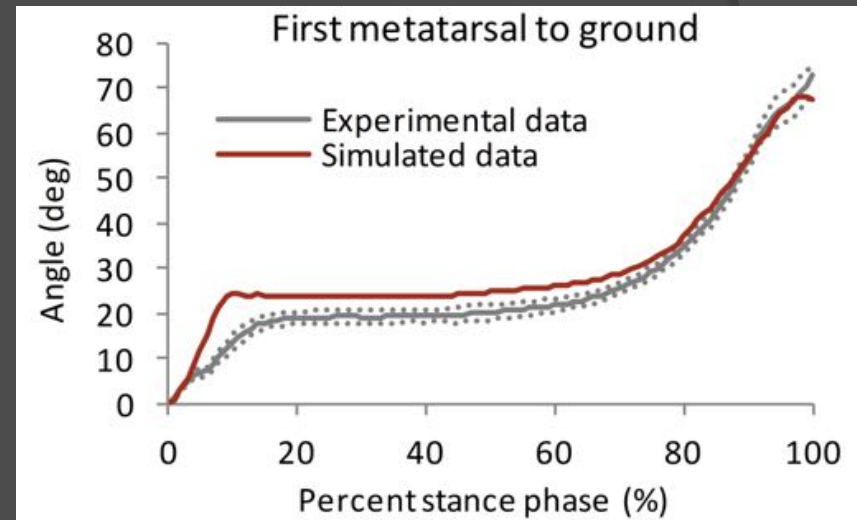


# Gait: Bone-to-ground angles

Normal



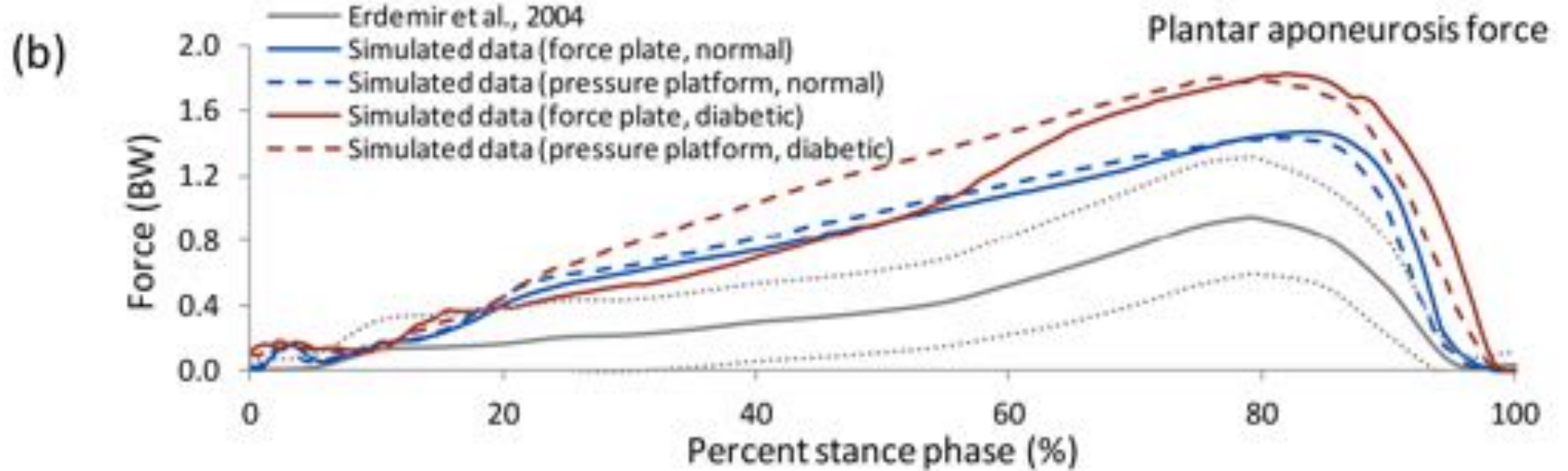
Diabetic





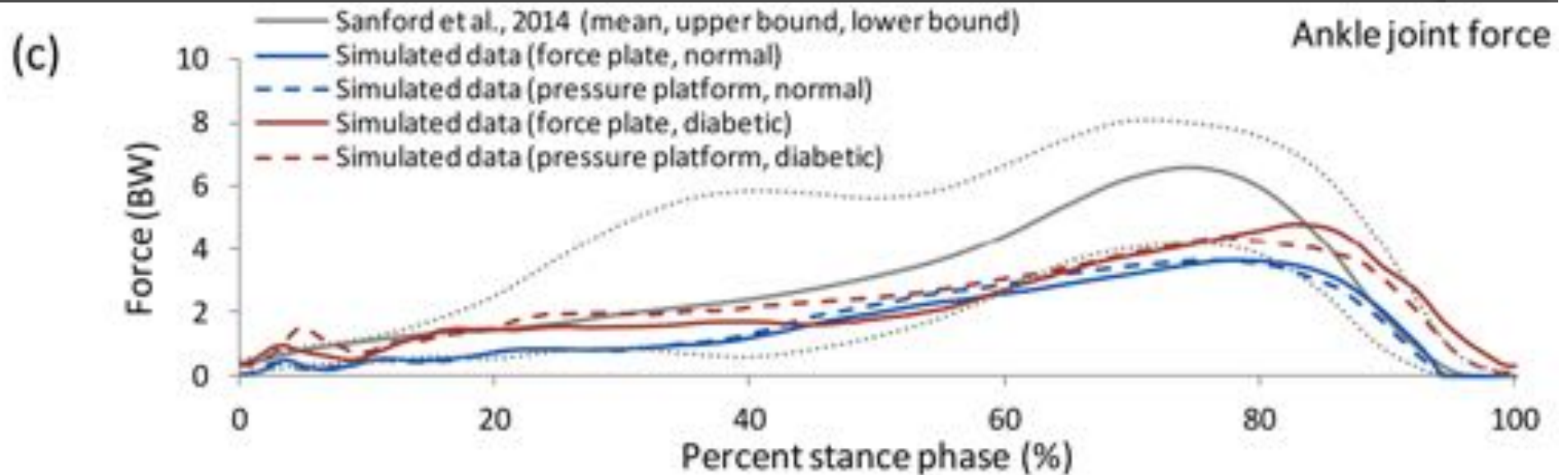
# Gait: Plantar fascia force

- Cadaveric experimental results vs FE model



# Gait: Ankle joint force

- In vivo inverse dynamic results vs FE model

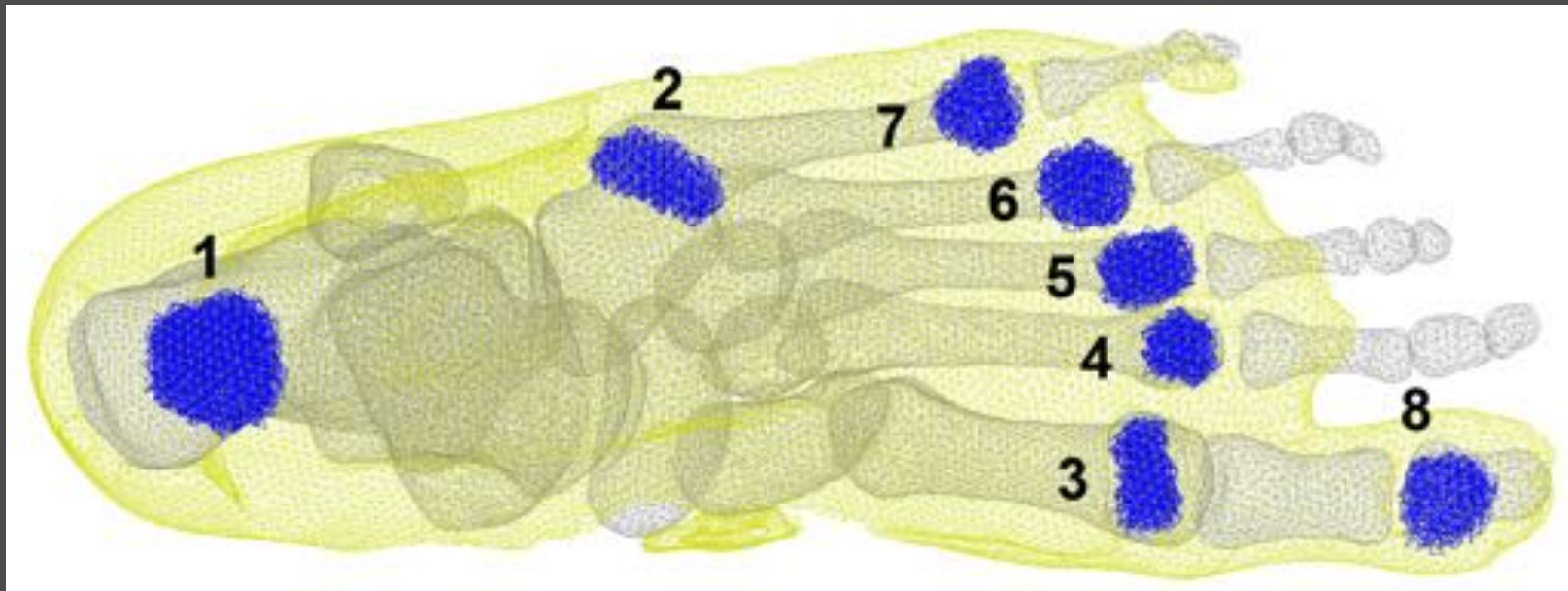


# Model prediction

- Internal stress
- Parametric analysis on the effect of soft tissue assumptions on plantar pressure and internal stress

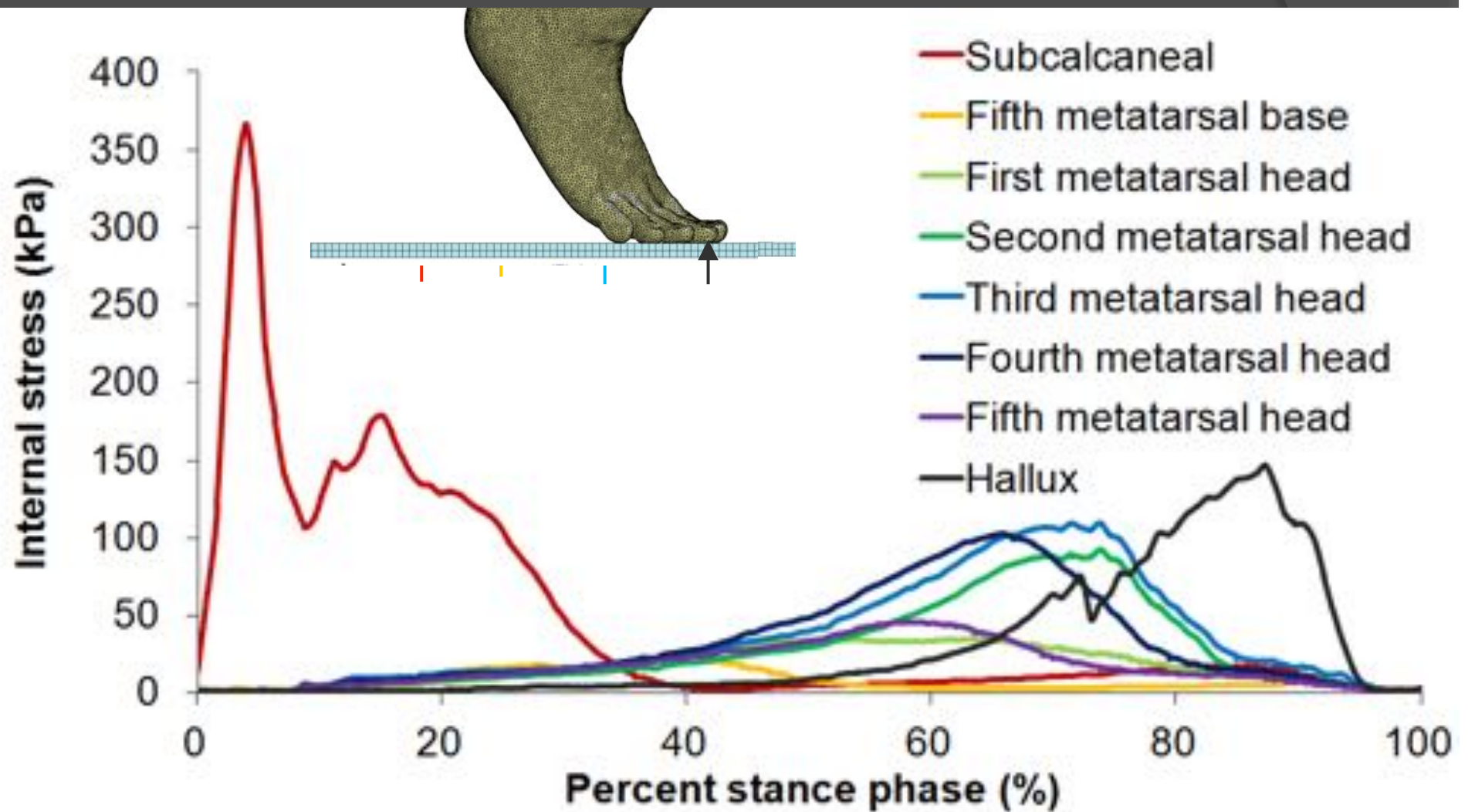
# Model prediction: Internal stress

- 8 locations in the plantar fat (ulcer risk locations)
- Calculated stress in terms of mean Von Mises stress<sup>1</sup>
- 1000 elements/region (3000 at the subcalcaneus)



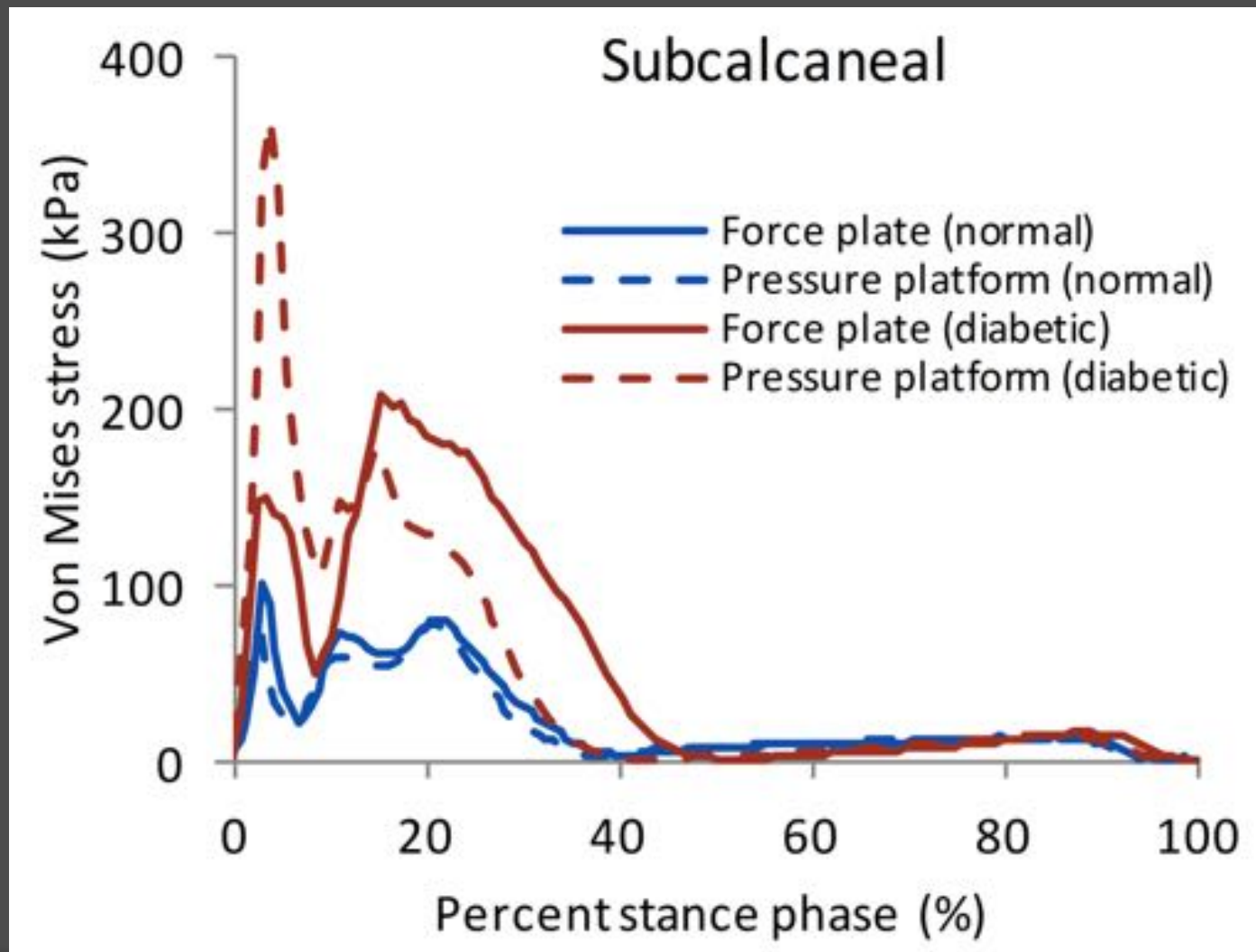
<sup>1</sup> [Gefen et al., 2003, *Med. Eng. Phys.*, 6: 491-499]

# Model prediction: Internal stress

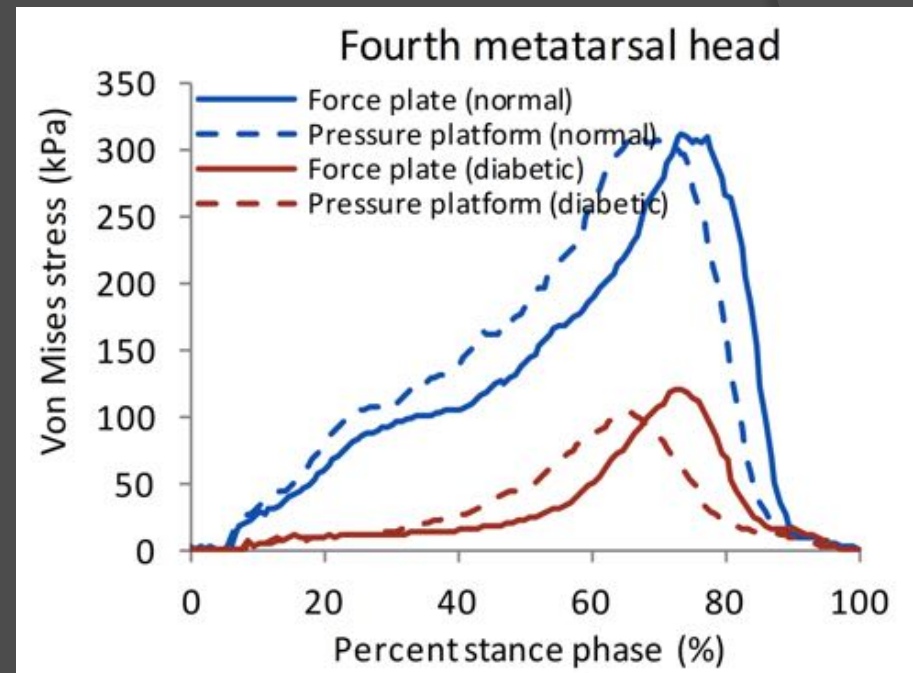
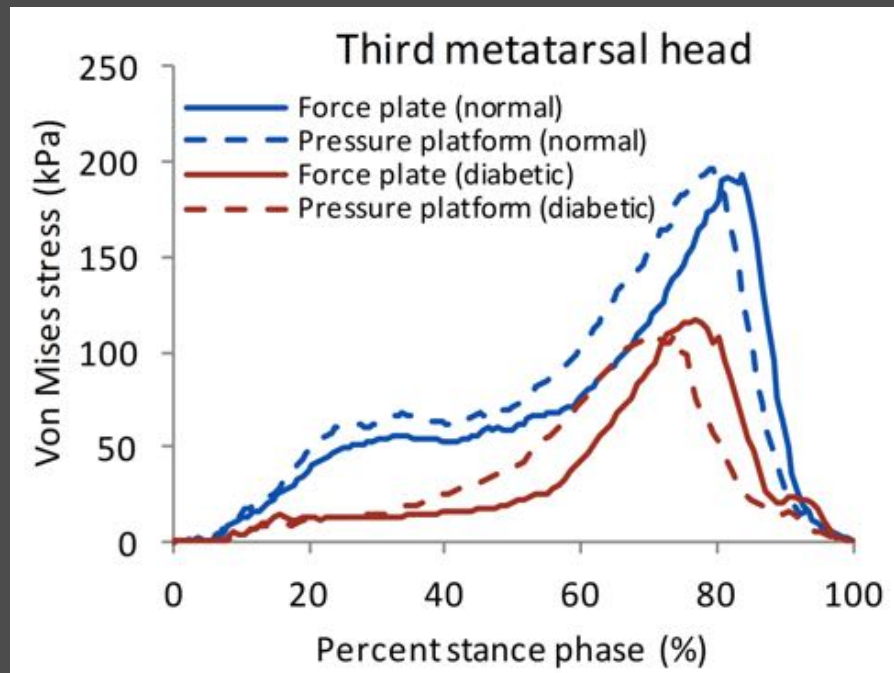




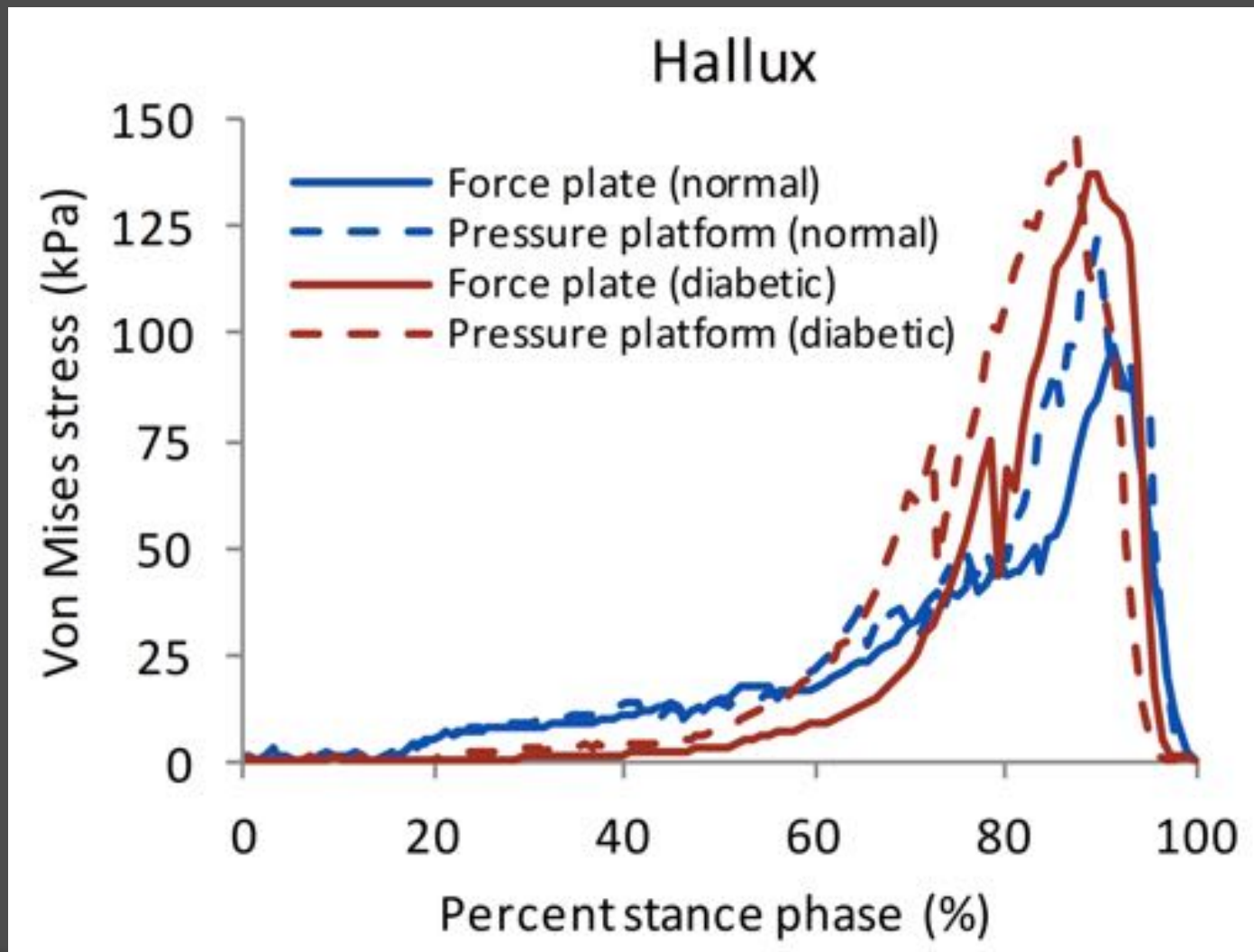
# Model prediction: Internal stress



# Model prediction: Internal stress



# Model prediction: Internal stress



# Model prediction: Parametric study

- ⦿ The effect of soft tissue material properties on plantar pressure and internal stress in quiet stance
  - 2X increased plantar fat stiffness
  - Generic soft tissue assumption
  - Non-subject-specific soft tissue assumption

# Quiet stance plantar pressure

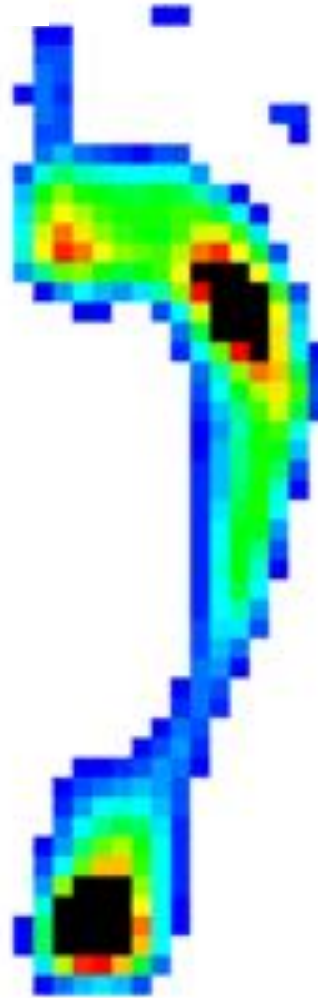
Baseline



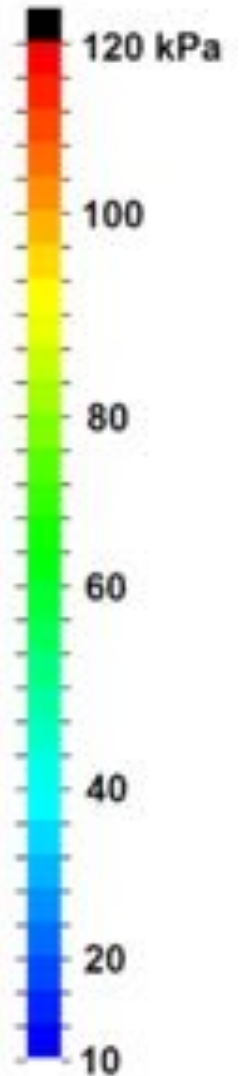
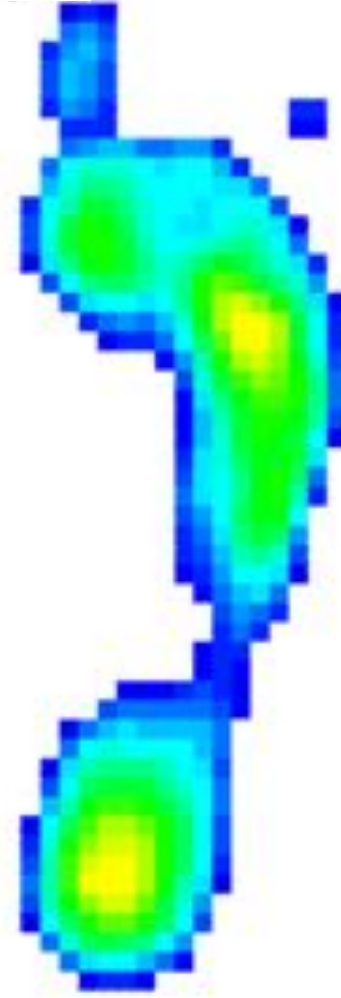
Increased  
plantar fat  
stiffness



Subject-specific  
generic soft  
tissue



Non-subject-  
specific material



# Conclusion

- ⦿ Subject-specific FE foot models
  - Subject-specific anatomy, soft tissue material properties and tibial kinematics
  - Improved plantar fascia component
  - Improved ligament, tendon structures and joint cavity
  - Extensive static and dynamic model validations