2D Signals and Systems

Signals

- A signal can be either continuous $f(x)$, $f(x,y)$, $f(x,y,z)$, $f(\mathbf{x})$
- or discrete $f_{i,j,k}^{\text{}}$ etc. where *i,j,k* index specific coordinates
- Digital images on computers are necessarily discrete sets of data
- Each element, or bin, or voxel, represents some value, either measured or calculated

Digital Images

- Real objects are continuous (at least above the quantum level), but we represent them digitally as an approximation of the true continuous process (pixels or voxels)
- For image representation this is usually fine (we can just use smaller voxels as necessary)

- For data measurements the element size is critical (e.g. Shannon's sampling theorem)
- For most of our work we will use continuous function theory for convenience, but sometimes the discrete theory will be required

Important signals - rect() and sinc() functions

• 1D rect() and sinc() functions

– both have unit area

Important signals - 2D rect() and sinc() functions

• 2D rect() and sinc() functions are straightforward generalizations

(a)
$$
\operatorname{rect}(x, y) = \begin{cases} 1, & \text{for } |x| < 1/2 \text{ and } |y| < 1/2 \\ 0, & \text{otherwise} \end{cases}
$$

\n(b) $\operatorname{sinc}(x, y) = \frac{\sin(\pi x) \sin(\pi y)}{\pi^2 xy}$

- *Try to sketch these*
- 3D versions exist and are sometimes used
- Fundamental connection between rect() and sinc() functions and very useful in signal and image processing

Important signals - Impulse function

Exponential and sinusoidal signals

• Recall Euler's formula, which connects trigonometric and complex exponential functions

$$
e^{j\theta} = \cos(\theta) + j\sin(\theta) \qquad \qquad \text{ (not i)}
$$

• The exponential signal is defined as:

 $e^{j2\pi x} = \cos(2\pi x) + j\sin(2\pi x)$, where $j^2 = -1$

- u_0 and v_0 are the fundamental frequencies in x and y directions, with units of 1/distance $e(x,y) = e^{j2\pi(u_0x + v_0y)}$
- We can write $e(x, y) = e^{j2\pi (u_0 x + v_0 y)}$

$$
= \cos \left[2\pi \left(u_0 x + v_0 y \right) \right] + j \sin \left[2\pi \left(u_0 x + v_0 y \right) \right]
$$

real and even **imaginary** and odd

Exponential and sinusoidal signals

• Recall that $\sin(2\pi x) =$ 1 2 *j* $\left(e^{j2\pi x}-e^{-j2\pi x}\right)$ $\cos(2\pi x) =$ 1 2 $(e^{j2\pi x} + e^{-j2\pi x})$

• so we have
$$
\sin[2\pi(u_0x+v_0y)]=\frac{1}{2j}(e^{j2\pi(u_0x+v_0y)}-e^{-j2\pi(u_0x+v_0y)})
$$

$$
\cos\left[2\pi\left(u_0x+v_0y\right)\right]=\frac{1}{2}\left(e^{j2\pi\left(u_0x+v_0y\right)}+e^{-j2\pi\left(u_0x+v_0y\right)}\right)
$$

- Fundamental frequencies u_0 , v_0 affect the oscillations in x and y directions, E.g. small values of u_0 result in slow oscillations in the xdirection
- These are complex-valued and directional plane waves

Exponential and sinusoidal signals

• Intensity images for $s(x,y) = \sin \left[2\pi (u_0 x + v_0 y) \right]$

 $u_0 = 1, v_0 = 0$

y

 $u_0 = 2, v_0 = 0$

 $u_0 = 4, v_0 = 0$

System models

- Systems analysis is a powerful tool to characterize and control the behavior of biomedical imaging devices
- We will focus on the special class of *continuous*, *linear*, *shiftinvariant* (LSI) systems
- Many (all) biomedical imaging systems are not really any of the three, but it can be useful tool, as long as we understand the errors in our approximation
- "all models are wrong, but some are useful" -*George E. P. Box*
- Continuous systems convert a continuous input to a continuous output

$$
g(x) = \mathscr{A}[f(x)] \quad (g(t) = \mathscr{A}[f(t)])
$$

$$
f(x) \rightarrow \mathscr{A} \rightarrow g(x)
$$

Linear Systems

• A system \mathscr{D} is a linear system if: we have $\mathscr{D} [f(x)] = g(x)$

then
$$
\mathscr{A}[a_1f_1(x) + a_2f_2(x)] = a_1g_1(x) + a_2g_2(x)
$$

or in general
$$
\mathscr{A}\left[\sum_{k=1}^K w_k f_k(x)\right] = \sum_{k=1}^K w_k \mathscr{A}\left[f_k(x)\right] = \sum_{k=1}^K w_k g_k(x)
$$

• Which are linear systems?

$$
g(x) = e^{\pi} f(x)
$$

$$
g(x) = f(x) + 1
$$

$$
g(x) = xf(x)
$$

$$
g(x) = (f(x))^{2}
$$

2D Linear Systems

- Now use 2D notation
- Example: sharpening filter

• In general

$$
\mathscr{A}\left[\sum_{k=1}^K w_k f_k(x,y)\right] = \sum_{k=1}^K w_k \mathscr{A}\left[f_k(x,y)\right] = \sum_{k=1}^K w_k g_k(x,y)
$$

Shift-Invariant Systems

then

• Start by shifting the input $f_{x_0y_0}(x, y) \triangleq f(x - x_0, y - y_0)$

if
$$
g_{x_0y_0}(x, y) = \mathscr{A}\Big[f_{x_0y_0}(x, y)\Big] = g(x - x_0, y - y_0)
$$

the system is *shift-invariant*, i.e. response does not depend on location

- Shift-invariance is separate from linearity, a system can be
	- shift-invariant and linear
	- shift-invariant and non-linear
	- shift-variant and linear
	- shift-variant and non-linear
	- (what else have we forgotten?)

Shift invariant and shift-variant system response

Shift invariant and shift-variant system response

Impulse Response

- Linear, shift-invariant (LSI) systems are the most useful
- First we start by looking at the response of a system using a point source at location (ξ, η) as an input

input
$$
f_{\xi\eta}(x, y) \triangleq \delta(x - \xi, y - \eta)
$$

output $g_{\xi\eta}(x, y) \triangleq h(x, y; \xi, \eta)$

- The output $h()$ depends on location of the point source (ξ, η) and location in the image (*x,y*), so it is a 4-D function
- Since the input is an impulse, the output is called the *impulse response function,* or the *point spread function* (PSF) - *why?*

Impulse Response of Linear Shift Invariant Systems

- For LSI systems $\mathscr{B}\left[f(x-x_0, y-y_0)\right] = g(x-x_0, y-y_0)$
- So the PSF is $\mathscr{B}\left[\delta(x-x_0, y-y_0)\right] = h(x-x_0, y-y_0)$
- Through something called the superposition integral, we can show that $g(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\xi,\eta) h(x,y;\xi,\eta) d\xi d\eta$ ∞ $\int_{-\infty}$ ∞ \int
- And for LSI systems, this simplifies to:

$$
g(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\xi,\eta) h(\xi - x, \eta - y) d\xi d\eta
$$

• The last integral is a convolution integral, and can be written as

$$
g(x, y) = f(x, y) * h(x, y) \quad (\text{or } f(x, y) * * h(x, y))
$$

Review of convolution

Properties of LSI Systems

- The convolution integral has the basic properties of
	- 1. Linearity (definition of a LSI system)
	- 2. Shift invariance (ditto)

3. Associativity
$$
g(x,y) = h_2(x,y) * [h_1(x,y) * f(x,y)]
$$

= $[h_2(x,y) * h_1(x,y)] * f(x,y)$

4. Commutativity $h_1(x, y) * h_2(x, y) = h_2(x, y) * h_1(x, y)$

Combined LSI Systems

- Parallel systems have property of
	- 5. Distributivity

$$
g(x,y) = h_1(x,y) * f(x,y) + h_2(x,y) * f(x,y)
$$

= $[h_1(x,y) + h_2(x,y)] * f(x,y)$

Summary of advantages of Linear Shift Invariant Systems

• For LSI systems we have $f(x,y) \rightarrow h(x,y)$ $\mapsto g(x,y)$

 $g(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\xi, \eta) h(\xi - x, \eta - y) d\xi d\eta$ ∞ $\int_{-\infty}$ ∞ \int $= f(x, y) * *h(x, y)$

object system image

- Treating imaging systems as LSI significantly simplifies analysis
- In many cases of practical value, non-LSI systems can be approximated as LSI
- Allows use of Fourier transform methods that accelerate computation

2D Fourier Transforms

Fourier Transforms

• Recall from the sifting property (with a change of variables)

$$
f(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\xi,\eta) \delta(\xi - x, \eta - y) d\xi d\eta
$$

- Expresses *f(x,y)* as a weighted combination of shifted basis functions, $\delta(x, y)$, also called the superposition principle
- An alternative and convenient set of basis functions are sinusoids, which bring in the concept of frequency
- Using the complex exponential function allows for compact notation, with *u* and *v* as the frequency variables

$$
e^{j2\pi(ux+vy)} = \cos\left[2\pi(ux+vy)\right] + j\sin\left[2\pi(ux+vy)\right]
$$

Exponential and sinusoidal signals as basis functions

• Intensity images for $s(x,y) = \sin \left[2\pi (u_0 x + v_0 y) \right]$

 $u_0 = 1, v_0 = 0$

 $u_0 = 2, v_0 = 0$

 $u_0 = 4, v_0 = 0$

 $u_0 = 4, v_0 = 1$

x

y

 $u_0 = 4, v_0 = 4$

Fourier Transforms

• Using this approach we write

$$
f(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} F(u,v) e^{j2\pi(ux+vy)} du dv
$$

- F(u,v) are the weights for each frequency, exp{ *j2*π*(ux+vy)*} are the basis functions
- It can be shown that using exp{ *j2*π*(ux+vy)*} we can readily calculate the needed weights by

$$
F(u, v) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-j2\pi(ux+vy)} dx dy
$$

• This is the 2D Fourier Transform of *f(x,y),* and the first equation is the inverse 2D Fourier Transform

Fourier Transforms

• For even more compact notation we use

 $F(u,v) = \mathcal{F}_{2D} \{ f(x,y) \}, \text{ and } f(x,y) = \mathcal{F}_{2D}^{-1} \{ F(u,v) \}$

- Notes on the Fourier transform
	- *F(u,v)* can be calculated if *f(x,y)* is continuous, or has a finite number of discontinuities, and is absolutely integrable
	- (u,v) are the spatial frequencies
	- *F(u,v)* is in general complex-valued, and is called the spectrum of *f(x,y)*
- As we will see, the Fourier transform allows consideration of an LSI system for each separate sinusoidal frequency

Fourier Transform Example

• What is the Fourier transform of • First note that it is separable • So we compute $rect(x, y) =$ 1, for $|x| < 1/2$ and $|y| < 1/2$ 0, otherwise $\begin{bmatrix} \end{bmatrix}$ $\left\{ \right.$ $\begin{cases} 0, & \text{otherwise} \end{cases}$ x *y* rect(*x,y*) $rect(x, y) = rect(x)rect(y)$ \mathcal{F}_{1D} {rect(*x*)} = \int rect(*x*)*e*^{-j2 π *ux*} $-\infty$ ∞ $\int \operatorname{rect}(x) e^{-j2\pi ux} dx$ $=$ $\int e^{-j2\pi ux}$ $-1/2$ 1/2 $\int e^{-j2\pi ux} dx =$ 1 $j2\pi u$ $e^{-j2\pi ux}$ $-1/2$ 1/2 = 1 π *u* $e^{j\pi u} - e^{-j\pi u}$ *j*2 = $sin(\pi u)$ π *u* $=$ sinc(*u*) Thus \mathcal{F}_{2D} {rect(*x*, *y*)} = sinc(*u*,*v*)

Fourier Transform Example

Two Key Properties of the 2D Fourier Transform

• Linearity
$$
\mathcal{F}_{2D}\left\{a_1f(x,y)+a_2g(x,y)\right\}=a_1F(u,v)+a_2G(u,v)
$$

• Scaling
$$
\mathcal{F}_{2D} \{ f(ax, by) \} = \frac{1}{|ab|} F\left(\frac{u}{a}, \frac{v}{b}\right)
$$

Signal localization in image versus frequency space

less localized

Fourier Transforms and Convolution

- Very useful! \mathcal{F}_{2D} $\{f(x,y) * g(x,y)\} = F(u,v)G(u,v)$
- Proof (1-D)

 $-\infty$

$$
\mathcal{F}\left\{f(x) * g(x)\right\} = \int_{-\infty}^{\infty} (f(x) * g(x))e^{-j2\pi ux} dx
$$

\n
$$
= \int_{-\infty}^{\infty} \left(\int_{-\infty}^{\infty} f(\xi)g(x-\xi) d\xi\right) e^{-j2\pi ux} dx = \int_{-\infty}^{\infty} f(\xi) \left(\int_{-\infty}^{\infty} g(x-\xi) e^{-j2\pi ux} dx\right) d\xi
$$

\n
$$
= \int_{-\infty}^{\infty} f(\xi) \left(\int_{-\infty}^{\infty} \mathcal{F}\left\{g(x-\xi)\right\}\right) d\xi = \int_{-\infty}^{\infty} f(\xi) \left(e^{-j2\pi u\xi} G(u)\right) d\xi
$$

\n
$$
= G(u) \int_{-\infty}^{\infty} f(\xi) e^{-j2\pi u\xi} d\xi = F(u)G(u)
$$

Fourier transform pairs

Signal

Fourier Transform

 $\mathbf{1}$ $\delta(x, y)$ $\delta(x-x_0, y-y_0)$ $\delta_s(x, y; \Delta x, \Delta y)$ $e^{j2\pi(u_0x+v_0y)}$ $\sin[2\pi (u_0x + v_0y)]$ $\cos [2\pi (u_0x + v_0y)]$ $rect(x, y)$ $sinc(x, y)$ $\text{comb}(x, y)$ $e^{-\pi(x^2+y^2)}$

 $\delta(u,v)$ $e^{-j2\pi(ux_0+vy_0)}$ $\text{comb}(u\Delta x, v\Delta y)$ $\delta(u - u_0, v - v_0)$ $\frac{1}{2i} \left[\delta (u - u_0, v - v_0) - \delta (u + u_0, v + v_0) \right]$ $\frac{1}{2} [\delta (u - u_0, v - v_0) + \delta (u + u_0, v + v_0)]$ $sinc(u, v)$ $rect(u, v)$ $\text{comb}(u, v)$ $e^{-\pi(u^2+v^2)}$

- Note the reciprocal symmetry in Fourier transform pairs
	- often 2-D versions can be calculated from 1-D versions by seperability
	- In general: a broad extent in one domain corresponds to a narrow extent in the other domain

Summary of key properties of the Fourier Transform

Transfer Functions

Transfer Function for an LSI System

• Recall that for an LSI system $f(x,y) \rightarrow g(x,y)$

$$
g(x,y) = f(x,y) * h(x,y) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(\xi, \eta) h(\xi - x, \eta - y) d\xi d\eta
$$

• We can define the **Transfer Function** as the 2D Fourier transform of the PSF

$$
H(u,v) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} h(\xi,\eta) e^{j2\pi(u\xi+v\eta)} d\xi d\eta = \mathcal{F}_{2D} \left\{ h(x,y) \right\}
$$

• In this case the LSI imaging system can be simply described by:

$$
g(x,y) = f(x,y) * h(x,y) = \mathcal{F}_{2D}^{-1} \{ F(u,v)H(u,v) \}
$$

• or
$$
G(u,v) = F(u,v)H(u,v)
$$

• which provides a very powerful tool for understanding systems

Illustration of transfer function $f(x,y) \rightarrow h(x,y) \rightarrow g(x,y)$

X-ray Radiography

Definitions

- Ion: an atom or molecule in which the total number of electrons is not equal to the total number of protons, giving it a net positive or negative electrical charge
- Radiation: a process in which energetic particles or energetic waves travel through a medium or space

Ionizing Radiation

- Radiation (such as high energy electromagnetic photons behaving like particles) that is capable of ejecting orbital elections from atoms
- Can also be particles (e.g. electrons)
- Ionizing energy required is the binding energy for that electron's shell
- Energy units are electron volts (eV or keV), the energy of an electron accelerated by 1 volt
- For Hydrogen K orbital electrons, *E*=13.6 eV
- For Tungsten K orbital electrons, *E*=69.5 keV
- In medical imaging we need photons with enough energy to transmit through tissue so are in range of 25 keV to 511 keV and is thus ionizing

Electrons as Ionizing Radiation

- Electron kinetic energy $E = (mv^2)/2$
- Three main modes of interaction in the energy range we are considering
	- a) Collision with other electrons and possible creation of delta-rays (high-energy electrons)
		- This is the most common mode and excited atoms loose energy by IR radiation (heat)
	- b) Ejection of an inner orbital electron
		- This orbit is filled by an outer electron and the difference in energy is released as a 'characteristic x-ray'
	- c) Bending of trajectory by nucleus
		- Since acceleration of a charged particle causes radiation, this causes 'braking radiation' or *bremsstrahlung*

X-ray Spectrum from Electron Bombardment

When high energy electrons hit tungsten (symbol W), three effects occur

- 1. Heat (> 99.9% of the energy)
- 2. Characteristic x-rays
- 3. Bremsstrahlung x-rays

